

## Study of a “wing-type” implant on stress distribution and bone resorption at the alveolar crest

Jong-Wook Park<sup>1</sup>, Sin-Guen Kim<sup>1</sup>, Dong-Won Choi<sup>2</sup>, Mi-Ra Choi<sup>3</sup>,  
Youn-Jin Yoon<sup>1</sup>, Jun-Woo Park<sup>1</sup>, Dong-Ju Choi<sup>1</sup>

<sup>1</sup>Department of Oral and Maxillofacial Surgery, College of Medicine, Hallym University, Chuncheon,

<sup>2</sup>Department of Beauty Skin Care, Kyungmin College, Uijeongbu,

<sup>3</sup>Department of Prosthodontics, College of Medicine, Hallym University, Chuncheon, Korea

**Abstract** (J Korean Assoc Oral Maxillofac Surg 2012;38:337-42)

**Objectives:** Implants connect the internal body to its external structure, and is mainly supported by alveolar bone. Stable osseointegration is therefore required when implants are inserted into bone to retain structural integrity. In this paper, we present an implant with a “wing” design on its area. This type of implant improved stress distribution patterns and promoted changes in bone remodeling.

**Materials and Methods:** Finite element analysis was performed on two types of implants. One implant was designed to have wings on its cervical area, and the other was a general root form type. On each implant, tensile and compressive forces (30 N/m<sup>2</sup>, 35 N/m<sup>2</sup>, 40 N/m<sup>2</sup>, and 45 N/m<sup>2</sup>) were loaded in the vertical direction. Stress distribution and displacement were subsequently measured.

**Results:** The maximum stresses measured for the compressive forces of the wing-type implant were 21.5979 N/m<sup>2</sup>, 25.1974 N/m<sup>2</sup>, 29.7971 N/m<sup>2</sup>, and 32.3967 N/m<sup>2</sup> when 30 N/m<sup>2</sup>, 35 N/m<sup>2</sup>, 40 N/m<sup>2</sup>, and 45 N/m<sup>2</sup> were loaded, respectively. The maximum stresses measured for the root form type were 23.0442 N/m<sup>2</sup>, 26.9950 N/m<sup>2</sup>, 30.7257 N/m<sup>2</sup>, and 34.5584 N/m<sup>2</sup> when 30 N/m<sup>2</sup>, 35 N/m<sup>2</sup>, 40 N/m<sup>2</sup>, and 45 N/m<sup>2</sup> were loaded, respectively. Thus, the maximum stresses measured for the tensile force of the root form implant were significantly higher (about three times greater) than the wing-type implant. The displacement of each implant showed no significant difference. Modifying the design of cervical implants improves the strength of bone structure surrounding these implants. In this study, we used the wing-type cervical design to reduce both compressive and tensile distribution forces loaded onto the surrounding structures. In future studies, we will optimize implant length and placement to improve results.

**Conclusion:** 1. Changing the cervical design of implants improves stress distribution to the surrounding bone. 2. The wing-type implant yielded better results, in terms of stress distribution, than the former root-type implant.

**Key words:** Dental implant, Wing, Modification

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### I. Introduction

The implant is designed to be connected to the inside of the human body and supported by alveolar bone. Since the implant should be maintained through adherence to bone, having it surrounded by healthy bone tissues is crucial.

In particular, the implant does not have periodontal ligament unlike natural teeth, and the stress exerted on it from

the outside may have different distribution pattern than that applied to natural teeth. Moreover, if the tissues surrounding the implant are inflamed, the inflammation spreads fast to the subsystem, and such is more likely to cause bone loss<sup>1</sup>.

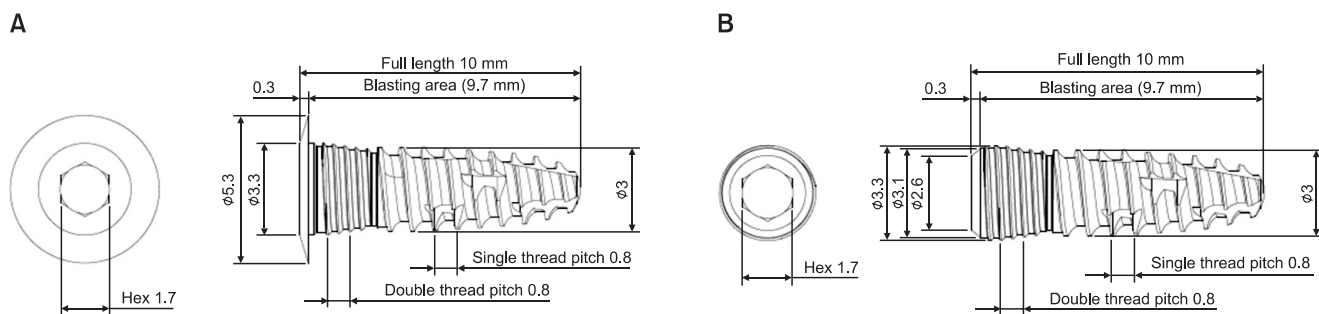
Therefore, it is very important that healthy bone tissues exist around the implant to ensure long-term maintenance. Nonetheless, there may be several unfavorable conditions that cause bone loss around the implant. There are many theories as to the reason implant cervical bone is absorbed and lost. Some of the factors considered include<sup>1</sup>: damage incurred during surgery<sup>2</sup>; overload generated by excessive occlusion<sup>3</sup>; inflammation around the implant<sup>4</sup>; small gaps between the fixture and abutment<sup>5</sup>; shaking caused by poor fixing of abutment<sup>6</sup>; biological width<sup>7</sup>, and; design of the implant neck<sup>8,9</sup> either separately or in combination.

Previously considered the standard, the Branemark implant

#### *Dong-Ju Choi*

Department of Dentistry, Hallym University Kangdong Sacred Heart Hospital,  
150, Seongan-ro, Gangdong-gu, Seoul 134-701, Korea  
TEL: +82-2-2224-2332 FAX: +82-2-483-9647  
E-mail: djcdavid@hanmail.net

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**Fig. 1.** Computer aided design (CAD) floor plan of two-type implants. A. Wide bevel-type (IS3010WB) CAD drawing. B. General root-type implant (IS3010G) CAD drawing.

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is known for its high rate of implant cervical bone absorption since it has all of the abovementioned factors. Thus, recently developed implant materials have stronger connection between the fixture and abutment to reduce shaking and minimize the stress exerted on the implant cervical bone.

The following are the ways of reducing the stress exerted on the cervical bone around an implant: increasing the number of implants used; using implants with larger diameters; improving the implant abutment design; improving the implant neck thread design, and; increasing the contact area between the implant and bone by expanding the implant surface area.

If the changes made to the implant neck to reduce the stress exerted on the cervical bone around the implant actually have an adverse effect on implant stability or biological width, the neck form should be improved to avoid such risks and contribute to bone formation.

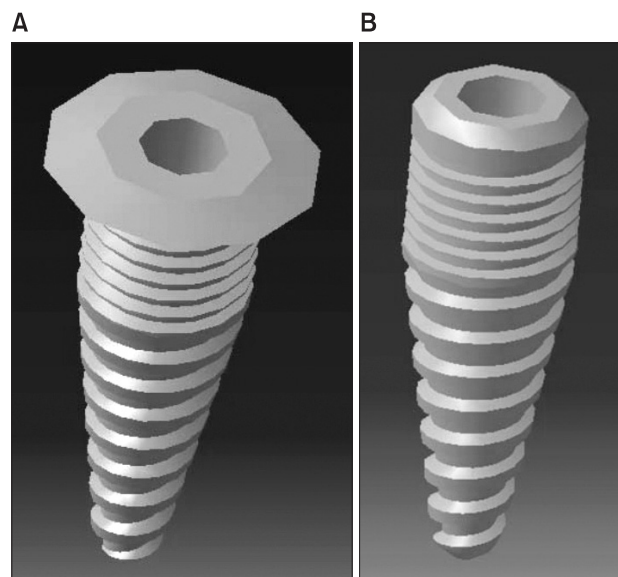
In this study, the distribution of stress exerted on the bone and the degree of bone formation facilitation were observed when implants with wing-shaped protrusions in the neck were used.

## II. Materials and Methods

### 1. Implant design

To reduce the stress exerted on the cervical bone around the implant, a wide bevel-type implant with protrusions on the cervical area was designed. Its plan was created with CATIA V5 (APuser, Seoul, Korea), a three-dimensional design program.(Figs. 1, 2)

1) Three dimensional (3D) structural design was done based on the drawing to analyze the structure of 2 types of implant structures presented.



**Fig. 2.** Two types of implants designed by CATIA V5. A. Wide bevel-type (IS3010WB) CATIA V5 plan. B. General root-type implant (IS3010G) CATIA V5 plan.

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2) Type 1 (wide bevel-type implant): submerged Implant wide bevel-type (IS3010WB)

Type 2 (general root-type implant): submerged implant general type (IS3010G)

- As shown in Fig. 1, the 3D design program CATIA V5 was used to execute the design in Fig. 2 based on a computer aided design drawing.

3) IS3010WB/IS3010G designed with CATIA V5 was manufactured with titanium, and CATIA V5 was used for structural interpretation to apply the mechanical material properties of titanium. The material properties applied are shown in Table 1.

4) After applying material properties, mesh work was done in the general structure for structural interpretation.

**Table 1.** Mechanical material properties of Ti for interpretation

Material	Titanium
Young modulus	$1.14 \times 10^{11} \text{ N/m}^2$
Poisson ratio	0.34
Density	$4,460 \text{ kg/m}^3$
Thermal expansion	0.0000095
Yield strength	$8.25 \times 10^8 \text{ N/m}^2$

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**Table 2.** IS3010WB mesh elements

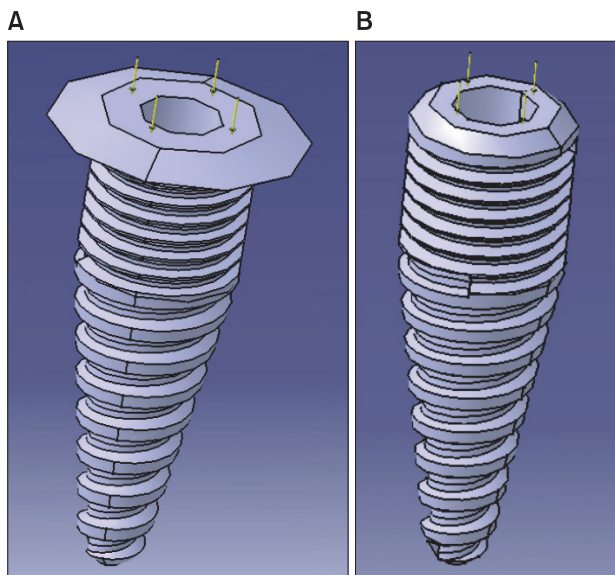
Entity	Size
Nodes	1,182
Elements	3,478

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**Table 3.** IS3010G mesh elements

Entity	Size
Nodes	1,229
Elements	3,799

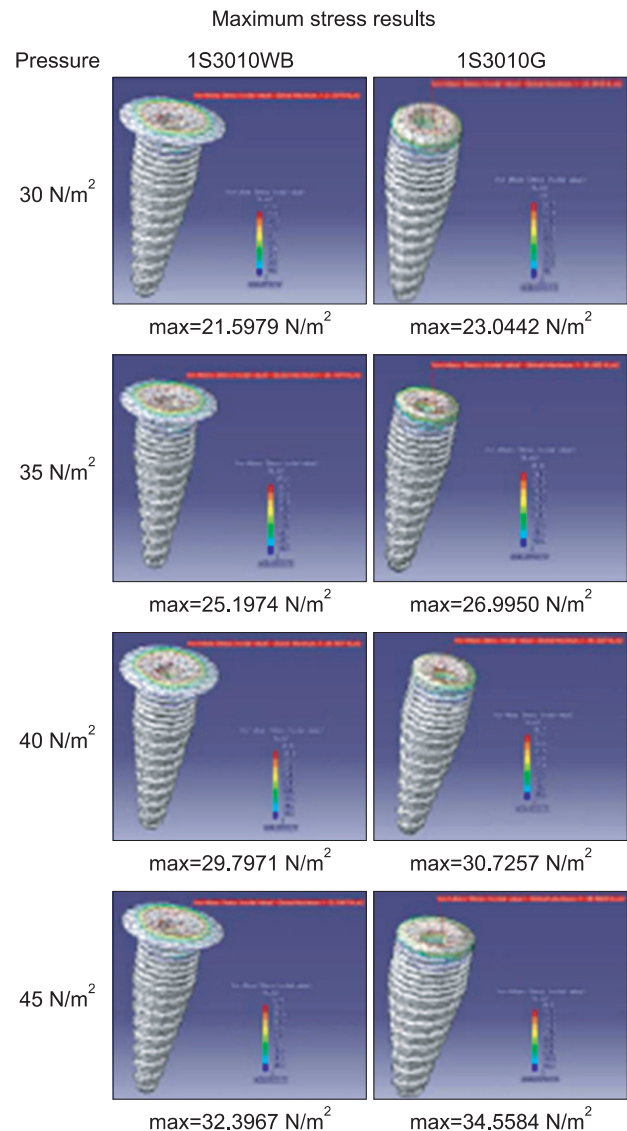
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**Fig. 3.** Force loaded to implant (yellow arrow). A. IS3010WB. B. IS3010G.

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The mesh elements of IS3010WB/IS3010G are shown in Tables 2, 3.

5) After the mesh work, forces of  $30 \text{ N/m}^2$ ,  $35 \text{ N/m}^2$ ,  $40 \text{ N/m}^2$ , and  $45 \text{ N/m}^2$  were exerted on the implant, and static analysis was performed during the use of finite element method (FEM).

**Fig. 4.** Finite element analysis (compressive force).

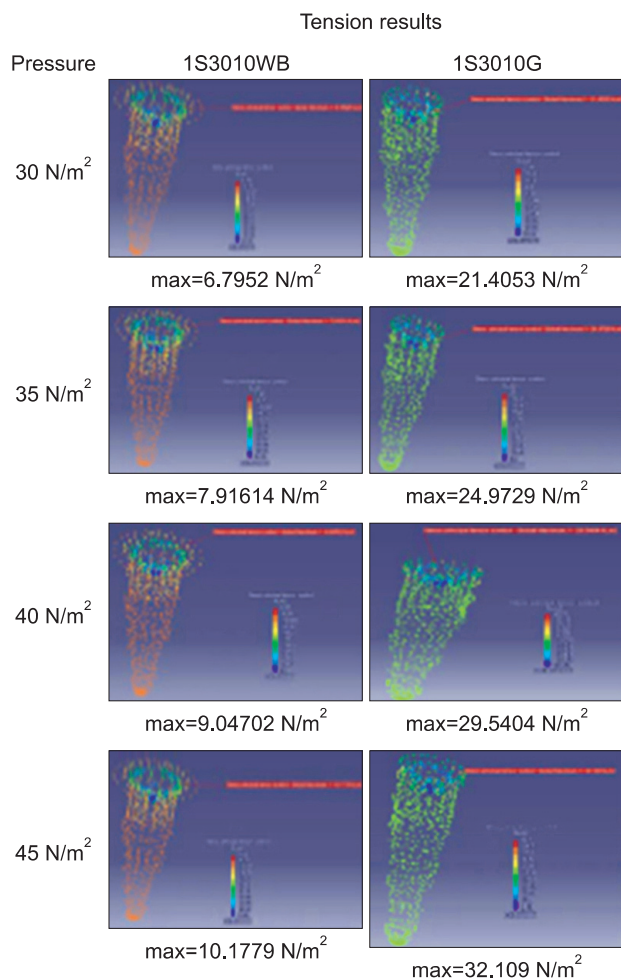
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The force exerted was vertical (Z axis) as shown in Fig. 3 from above the implant (indicated by the yellow arrow); both pressure and tension were exerted, and displacement was measured accordingly.

### III. Results

Each implant received force of  $30 \text{ N/m}^2$ ,  $35 \text{ N/m}^2$ ,  $40 \text{ N/m}^2$ , and  $45 \text{ N/m}^2$ . The results of such application of force on 2 types of implants are shown in Figs. 4-6.

When maximum stress was applied, the structural displacement made to 2 types of implants (Fig. 4) caused almost no change to the upper structure of the wide bevel-type implant as stress increased ( $30 \text{ N/m}^2$ ,  $35 \text{ N/m}^2$ ,  $40 \text{ N/m}^2$ ,



**Fig. 5.** Finite element analysis (tensile force).

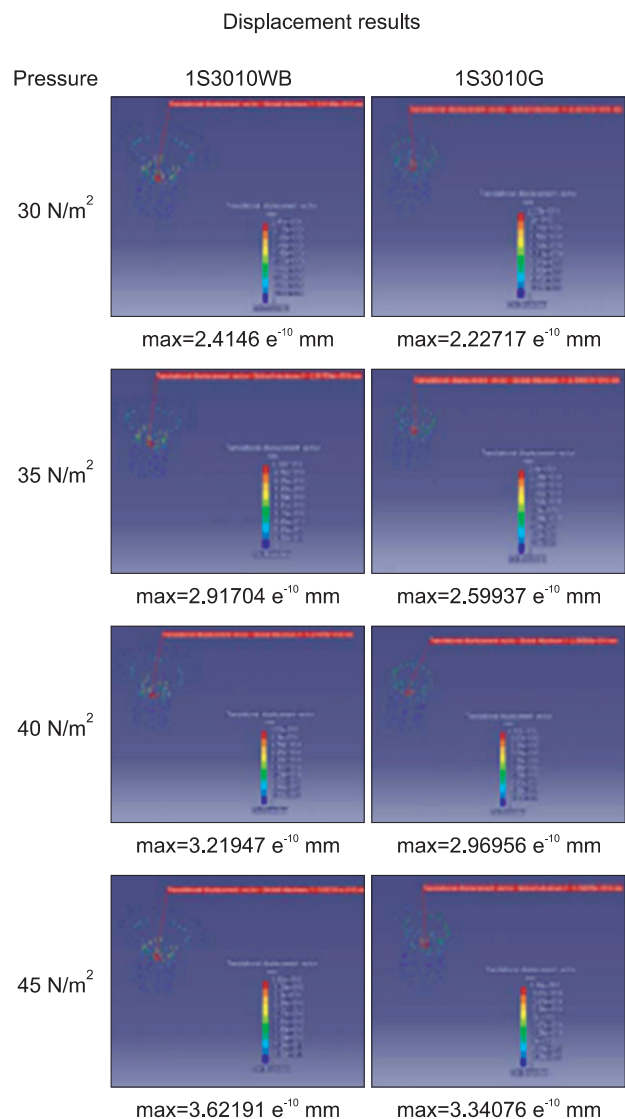
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and 45 N/m<sup>2</sup>) as well as evident gradual deformation on the tapped part of the general root-type implant.

When maximum stress was applied, the maximum forces measured at the mesh were 21.5979 N/m<sup>2</sup>, 25.1974 N/m<sup>2</sup>, 29.7971 N/m<sup>2</sup>, and 32.3967 N/m<sup>2</sup> for the wide bevel-type implant and 23.0442 N/m<sup>2</sup>, 26.9950 N/m<sup>2</sup>, 30.7257 N/m<sup>2</sup>, and 34.5584 N/m<sup>2</sup> for the general root-type implant in response to stress of 30 N/m<sup>2</sup>, 35 N/m<sup>2</sup>, 40 N/m<sup>2</sup>, and 45 N/m<sup>2</sup>.

The forces measured when tension was exerted were 6.7952 N/m<sup>2</sup>, 7.9161 N/m<sup>2</sup>, 9.0470 N/m<sup>2</sup>, and 10.1779 N/m<sup>2</sup> for the wide bevel-type implant and 21.4053 N/m<sup>2</sup>, 24.9729 N/m<sup>2</sup>, 29.5404 N/m<sup>2</sup>, and 32.1090 N/m<sup>2</sup> for the general root-type implant.

The forces measured when stress was exerted were 2.4246 e<sup>-10</sup> mm, 2.9170 e<sup>-10</sup> mm, 3.2195 e<sup>-10</sup> mm, and 3.6219 e<sup>-10</sup> mm for the wide bevel-type implant and 2.2272 e<sup>-10</sup> mm, 2.5994 e<sup>-10</sup> mm, 2.9696 e<sup>-10</sup> mm, and 3.3408 e<sup>-10</sup> mm for the general root-type implant.



**Fig. 6.** Finite element analysis (displacement).

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As shown in the result above, the wide bevel-type distributes average pressure of 2 N/m<sup>2</sup> better than the general root-type does.

This implies that the wide bevel-type implant (IS3010WB) distributes pressure to the Z axis from the upper structure more effectively than the general root-type implant (IS3010G) does.

In addition, the result concerning tension (Fig. 5) shows that the wide bevel-type implant distributes pressure three times better than its counterpart with far better structure stability.

In terms of displacement, Fig. 6 presents the structural changes in response to pressure in length. Note, however, that this figure is too small to show displacement smaller than e<sup>-10</sup>



mm; thus, the difference was not significant.

The overall result suggests that the wide bevel-type implant is far better than the general root-type implant in terms of pressure distribution.

#### IV. Discussion

Continuous efforts are being made to ensure stability in the cervical bone after implanting. To do so, the surface shape of the implant is changed to reduce the time needed for integration to bone, bonded bone strength is increased for greater stability, fine thread is made in the implant neck to minimize bone loss, and one-body implant is made to prevent the shaking of the abutment or increase biological width. In many cases, the implant neck is designed differently to transfer stress most efficiently.

Chung et al.<sup>1</sup> observed the change of stress exerted on the cervical bone with FEM with two types of implants - Nobel Biocare's NobelDirect and Straumann's ITI - which had a straight form among other one-body implants. The result suggests that the stress exerted is reduced if the neck penetrating is curved rather than straight.

Bozkaya et al.<sup>10</sup> used 5 types of widely used implants (Ankylos, Astra, Bicon, ITI, and Nobel Biocare) for analysis based on FEM and observed the force transferred to the surrounding bone when occlusive force was exerted. They exerted overload for vertical, lateral, and shearing forces and in the general occlusive direction (11.3°; occlusion to 1 mm from the central axis of the implant) to see which type of implant delivered the highest overload to the surrounding bone. The result showed that ITI was the one that transferred most stress to the surrounding bone. This test also suggested that various types of forces exerted on the implant were mostly delivered to the bone surrounding the implant neck.

According to Geng et al.<sup>11</sup>, the factors affecting the mechanism delivering force to the interface between the alveolar bone and implant included the type of force, material properties of the implant and prosthetic appliance, shape of the implant, and structure of the surface, among others.

Their study found that the layered structure delivered force in a more uniform manner compared to the straight, cylindrical design. In particular, such requirements were deemed to have been met by changing the size, shape, material, and surface of the implants, and some of them were developed prior to fundamental research<sup>12</sup>.

Abu-Hammad et al.<sup>13</sup> made implant surfaces whose cross section was smooth or spiral- or star-shaped and analyzed

the stress exerted by such implants on the surrounding bone. According to them, the implant with no change made to the surface exerted the least stress. Personally, however, the authors believe that this maximizes friction against surrounding bone, and that it is impossible to use in actual cases.

Today's implant neck designs are in many ways significant and are studied from the esthetic or stability point of view. In particular, Bischof et al.<sup>14</sup> used ITI implants of the same properties with 4.8 mm and 6.5 mm neck for a comparative analysis. The wider one reportedly causes less bone loss.

In this study, too, we widened the implant neck for better stress distribution. The wide bevel-type neck design in particular minimizes the displacement of the implant itself and the stress exerted by the displacement force on the surrounding bone when implanted. This is a very important point, indicating that the local stress exerted on the interface between the implant and bone is related to bone loss.

Moreover, the protrusions in the neck act as an umbrella that prevents the soft body in the bottom from growing upward and facilitates bone formation at the bottom. Even though the implant is in contact with poor-quality bone in the implanting procedure, it is considered to contribute to the success rate of the procedure since bone formation is facilitated from the bottom.

#### V. Conclusion

1. Changing the implant neck design affects the distribution of force exerted on the surrounding bone.

This result is deemed to affect the displacement of the implant itself and the amount of force exerted on the surrounding bone and ultimately on the absorption of the surrounding bone.

2. The wide bevel-type distributes force better than the standard implant and prevents soft body penetration from below the protrusions; thus facilitating bone formation and expanding the contact area of the implant and alveolar bone.

3. Note, however, that the protrusions should have minimum effective length since they are inferior from an esthetic point of view.

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