

Shear bond strength of dentin bonding agents cured with a plasma arc curing light

Youngchul Kwon, Sun-Young Kim, Sae-Joon Chung, Young-Chul Han, In-Bog Lee,
Ho-Hyun Son, Chung-Moon Um, Byeong-Hoon Cho*

*Department of Conservative Dentistry & Dental Research Institute, School of Dentistry,
Seoul National University*

ABSTRACT

The objective of this study was to compare dentin shear bond strength (DSBS) of dentin bonding agents (DBAs) cured with a plasma arc (PAC) light curing unit (LCU) and those cured with a light emitting diode (LED) LCU. Optical properties were also analyzed for Elipar freelight 2 (3M ESPE); LED LCU, Apollo 95E (DMT Systems); PAC LCU and VIP Junior (Bisco); Halogen LCU. The DBAs used for DSBS test were Scotchbond Multipurpose (3M ESPE), Singlebond 2 (3M ESPE) and Clearfil SE Bond (Kuraray). After DSBS testing, fractured specimens were analyzed for failure modes with SEM.

The total irradiance and irradiance between 450 nm and 490 nm of the LCUs were different. LED LCU showed narrow spectral distribution around its peak at 462 nm whereas PAC and Halogen LCU showed a broad spectrum. There were no significant differences in mean shear bond strength among different LCUs ($P > 0.05$) but were significant differences among different DBAs ($P < 0.001$) [J Kor Acad Cons Dent 33(3):213-223, 2008]

Key words : PAC, LED, Dentin bonding agent, Spectral irradiance, Energy density, Dentin shear bond strength

- Received 2008.2.28., revised 2008.3.7., accepted 2008.4.29. -

I . INTRODUCTION

Proper performance of light curing unit is prerequisite to produce resin restorations with optimal physical properties and clinical results. The most common light-curing source used in dentistry is the Quartz

Tungsten Halogen (QTH) light¹⁾. Halogen light bulbs generate light by electrically heating tungsten thread to temperatures of some thousands of degrees centigrade²⁾. Even though QTH lights have some reliability from their long history of clinical usage, their inherent drawbacks have been pointed out by numerous authors^{2-5,7)}. For example, the halogen bulbs have a limited life time of approximately 40 to 100 hours. In addition, reflector and filter degrade over time due to the high operating temperatures and the large quantity of heat which is produced during the duty cycles³⁾.

* Corresponding Author: **Byeong-Hoon Cho**

Dept. of Conservative Dentistry & Dental Research
Institute, School of Dentistry, Seoul National University,
28-2 Yeongon-Dong, Chongno-Ku, Seoul, 110-749, Korea
Tel: 82-2-2072-2651 Fax: 82-2-2072-3859
E-mail: chobh@snu.ac.kr

※ This study was supported by SNUH FUND 04-2006-0007.

To overcome the problems inherent to QTH, solid state light emitting diode (LED) technology has been proposed for curing light-activated dental materials⁴⁾. The spectral output of gallium nitride blue LEDs falls conveniently within the absorption spectrum of the camphorquinone photoinitiator (400 - 500 nm) present in light-activated dental materials, so no filters are required in LED light curing unit (LCU)s. Furthermore, LEDs have an expected lifetime of several thousand hours without significant degradation of light emission over time⁵⁾. However, LEDs can only polymerize the products utilizing camphorquinone as the photoinitiator since the spectral distribution of all currently available LEDs, except some third generation LEDs like Ultralume 5 which has wider spectral range, is narrow^{6,7)}. Also, speed of cure using LED is still inferior to Plasma Arc Curing (PAC) light.

Instead of a filament, PAC lights contain two tungsten electrodes separated by a small gap. High voltage is generated between electrodes. The resulting spark ionizes the gaseous environment (Xenon) and creates a conductive gas known as plasma⁸⁾. Even with the optical losses of the waveguide, necessary because of the high voltage present at the bulb, higher light intensities can be obtained with PAC light²⁾. The advent of the PAC light brought criticism from some researchers who felt that it cured resin too fast, and that subsequent damage to tooth structure and resin would result. However, PAC's speed of cure and the resultant immediate continuity of steps in any resin placement procedure are unequaled by other types of currently popular lights⁹⁾.

There are numerous studies on PAC lights. Unfortunately however, there are few studies on bond strength of dentin bonding agents cured with PAC lights in restorative dentistry. Therefore, the purpose of this study was to analyze optical properties of PAC lights compared with Halogen and LED lights and to evaluate curing effectiveness of PAC lights by comparing shear bond strengths of dentin bonding agents cured with either PAC or LED lights. The hypothesis was that the bond strength of dentin bonding agents cured with PAC for 3 seconds would be lower than those of dentin bonding agents cured with either PAC for 6 seconds or LED for 10 seconds.

II . MATERIALS AND METHODS

1. Optic characterisitcs

Three commercially available lights were evaluated for their optic characteristics. Apollo 95E (DMT Systems, CA, USA), Elipar FreeLight 2 (3M ESPE, MN, USA) and VIP junior (Bisco, IL, USA) were selected to represent PAC, LED and QTH light, respectively. The guide tip diameter of Apollo 95E and Elipar Free Light 2 was 8 mm whereas that of VIP junior was 10 mm. The power outputs of each LCU were measured using EPM 1000 power meter with PM30 thermopile sensor (Moletron Detector Inc., Oregon, USA) which has a measuring wavelength range of 190 - 11,000 nm and a calibration uncertainty of 1 %. The power output values were converted to the power density values (in mW/cm²) by dividing it with the area of the LCU light guide tip. The power densities obtained with EPM 1000 power meter were compared with the values reported by manufacturers and those measured with portable radiometers. Optilux (Kerr, CA, USA) was used as simple radiometer for Elipar FreeLight 2 and VIP Junior, and EFOS hand-held radiometer (EFOS Inc., Ontario, Canada) was used for Apollo 95E because Optilux could measure light intensity only up to 1000 mW/cm².

The spectral distributions of the LCUs were obtained using MS 257 monochromator with Andor CCD array detector (Oriel Ins., CT, USA). The y-axis unit value of each LCU was determined by the equations between total irradiance value obtained by Moletron EPM 1000 and the integrated sum of the LCU's spectrum. The power densities in the ranges of 410 - 500 nm and 450 - 490 nm were obtained by integration of the spectrum in each range. Integration of the spectrum was performed using an Origin 7.0 program (Original lab Corporation, MA, USA). The calculation procedures are shown below. :

$$P[\text{mW}], A[\text{cm}^2]$$

$$I(\text{Power density}) = P[\text{mW}]/A[\text{cm}^2]$$

$$Y[\text{mW}/\text{cm}^2/\text{nm}] = F(\lambda)[\text{mW}/\text{cm}^2/\text{nm}]$$

$$y = f(\lambda) = \int F(\lambda)d\lambda = I$$

$$F(\lambda) = Cf(\lambda)$$

$$Cf(\lambda)d\lambda = I, C = I/\int f(\lambda)d\lambda$$

I: Integrated sum from the spectrum of PAC, LED and Halogen respectively (Total intensity)

Y: Real y axis unit of spectrum

2. Shear bond strength test

135 freshly extracted caries free human third molars were collected, stored at 4°C in 0.5 % chloramine-T solution for 1 week and then in distilled water for no longer than 3 months until performing shear bond test. Cylinder shape acrylic molds were prefabricated. The dimensions for the mold were 25 mm in outer diameter and in height, and the dimensions for inner hole of the mold to accommodate tooth

were 15 mm (diameter) and 10 mm (height). After the embedding procedure, the specimen (tooth in the mold) was allowed to sit for five minutes for exothermic reactions and stored in the distilled water.

The embedded teeth were sectioned through mid-crown parallel to their occlusal surface to expose the dentin surface using a low-speed diamond saw (Isomet, Buehler, IL, USA) under running water. The exposed dentin surface was polished with 500 grit silicon carbide papers under water irrigation using an automatic polishing machine (Rotapol-V, Struers, Glasgo, UK).

135 prepared specimens were randomly divided into 9 groups of 15 teeth. The 9 groups consists of 3

Table 1. Components and bonding procedures of the dentin bonding systems and composites used in this study

Bonding systems	Code	Components	Bonding procedures	Resin composites
Scotchbond Multipurpose (Etchant: Lot:5FY) (Primer: Lot:6BE) (Adhesive: Lot: 6pp)	MP	Primer: Water, HEMA, Copolymer of acrylic and itaconic acids. Adhesive: Bis-GMA, HEMA, Photoinitiator.	Etched with 35% H ₃ PO ₄ for 15s. Rinsed, dried with a gentle air. Primer applied, dried gently. Adhesive applied. Light-cured for 10s.	Filtek Z250 (A2 shade) (Lot:6LNJ)
Single Bond2 (Lot: 6JH)	SB	Ethyl alcohol, Bis-GMA, HEMA, Silica nanofiller, Water, Glycerol 1,4-dimethacrylate, Photoinitiator, Copolymer of acrylic and itaconic acids, Diurethane dimethacrylate.	Etched with 35% H ₃ PO ₄ for 15s. Rinsed, excess water blotted. Adhesive applied in two consecutive coats. Agitated 15s, air-thinned to evaporate the solvent. Light cured for 10s.	Filtek Z250 (A2 shade) (Lot:6LNJ)
Clearfil SE Bond (Self etching primer: Lot:00723A) (Adhesive: Lot:01039A)	SE	Primer: MDP, HEMA, water, Hydrophilic dimethacrylate, N,N-Diethanol-p-toluidiene. Adhesive: MDP, Bis-GMA, HEMA, Hydrophobic dimethacrylate, N,N-Diethanol-p-toluidiene, Silicated colloidal silica.	Dried with light air. SE primer applied, wait for 20s. Evaporate volatile ingredients. Adhesive applied, gently air-streamed to make a uniform adhesive film. Light cured for 10s.	Clearfil AP-X (A2 shade) (Lot:0091A)

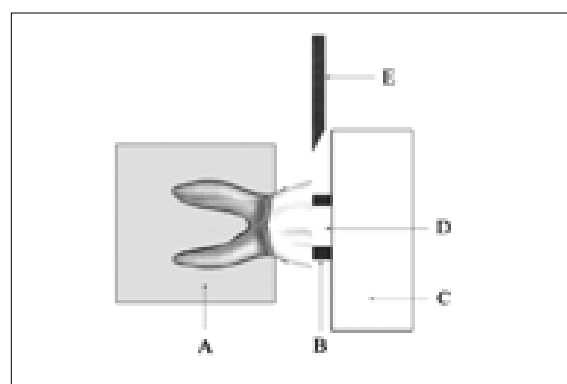
Table 2. The groups tested in this study

	PAC 3s/3s Apollo 95E	PAC 6s/6s Apollo 95E	LED 10s/20s Elipar Freelight 2
Scotchbond Multipurpose (MP) with Z250	MP-P3	MP-P6	MP-L
Single Bond (SB) with Z250	SB-P3	SB-P6	SB-L
Clearfil SE Bond (SE) with AP-X	SE-P3	SE-P6	SE-L

Dentin Bonding Agent(DBA)s cured with 3 curing modes. The 3 DBAs used in this study were a 3-step total etching DBA system, Scotchbond Multipurpose (MP, 3M ESPE, USA); a 2-step total etching DBA system, Single Bond 2 (SB, 3M ESPE, USA); and a 2-step self-etching DBA system, Clearfil SE Bond (SE, Kuraray Medical, Japan). The information and bonding procedures for each DBA are listed in Table 1 and the assignment for 9 groups is shown in Table 2.

Each DBA was applied on the middle of the exposed dentin surface according to manufacturer's recommendation, trying to confine the bonded area to be less than 6 mm diameter which is the outer diameter of the metal iris and cured with either Apollo 95E for 3 seconds, Apollo 95E for 6 seconds or Elipar FreeLight 2 for 10 seconds at a distance of 1 mm from the light guide tip. A Teflon-coated metal iris with a 3 mm internal diameter, 6 mm outer diameter and 1.5 mm height was used as a mold for composite. The metal iris, which was held in an acrylic cap, was pressed against the bonded dentin surface and the cavity made by iris was filled with the same manufacturer's composite corresponding to each DBA. This composite placed on the top of the previously cured DBA was cured with either Apollo 95E for 3 seconds, Apollo 95E for 6 seconds or Elipar FreeLight 2 for 20 seconds, with the light guide tip in direct contact with the metal iris. This specimen was allowed to sit for additional 4 minutes and stored in distilled water at room temperature for 24 hours before testing.

The specimens were loaded in shear mode to failure in a universal testing machine (LF Plus, Lloyd

**Figure 1.** Schematic diagram of metal iris assembly supported with Teflon wall.

A, Embedding resin; B, Teflon coated metal iris; C, Teflon wall; D, Resin composite; E, Load application chisel

Instruments Ltd., Hampshire, UK) at a crosshead speed of 2 mm/minute by using a knife edged chisel that was pressed as close as possible to the edge of the metal iris adjacent to the bonded tooth surface. This technique is shown schematically in Figure 1. The shear bond strength was calculated in MPa by dividing the maximum load (Newtons) by the cross sectional area of the bonded surface. Following the shear bond strength test, all the fractured dentin surfaces were observed under Operating microscope (OPMI 111, Carl Zeiss, Germany) at $\times 21$ magnification to determine their fracture modes. Some specimens were randomly selected, placed on the field-emission scanning electron microscopy (FE-SEM) stub followed by gold-sputter coating and were observed under FE-SEM (S-4700, Hitachi, Japan) to show illustrative FE-SEM shapes of the fractured

dentin surfaces. Failure mode was classified into 4 types:

Type 1: failure between adhesive and dentin

Type 2: mixed pattern of adhesive failure and cohesive failure in composite or dentin combined

Type 3: cohesive failure in composite

Type 4: cohesive failure in dentin

After the residual analysis which revealed the equality of variance, two-way analysis of variance was used to analyze whether there are differences in the shear bond strength. Differences among the groups were assessed using Bonferroni's multiple comparison tests. A probability value of < 0.05 was considered significant.

III. RESULTS

The light irradiance of the LCUs reported by manufacturers and measured in this study with hand-held radiometer and EPM 1000 is shown in Table 3. The

spectral distributions of LCUs obtained with MS 257 monochromator are shown in Figure 2(a). The total area and the area in the region of 450 - 490 nm and 410 - 500 nm under each curve represent the total irradiance and irradiance in the corresponding region. The irradiance in each region is shown as graph in Figure 2(b).

The means of shear bond strength were shown in Table 4 and Figure 3. There were significant differences in the mean values of shear bond strength among different DBAs ($p < 0.001$). However, there were no significant differences among the different LCUs ($p > 0.05$). The interaction between DBA and LCU was not significant. Failure modes of the fractured dentin surfaces are shown in Figure 4. The FE-SEM shapes of fractured specimens were shown in Figure 5(a), 5(b) and 5(c). Mixed failure was the most predominant failure mode followed by adhesive failure. There were only 3 cases of composite cohesive failures and no extensive dentin cohesive failure.

Table 3. Light irradiance (mW/cm^2) measurements

	Manufacturer	Optilux and EFOS radiometer	EPM 1000 Power meter
Apollo 95E (Plasma Arc Light)	About 2000	1710	2307
Elipar Freelight 2 (LED)	About 1000	800	805
VIP Junior (QTH)	About 600	580	674

Table 4. Mean shear bond strength (MPa) of DBAs cured with PAC and LED

PAC 3s/3s	PAC 6s/6s	LED 10s/20s	
MP	22.7 ± 4.85^a	$24.1 \pm 6.2^{a,b}$	$26.7 \pm 6.17^{a,b}$
SB	$24.4 \pm 4.28^{a,b}$	$24.3 \pm 6.3^{a,b}$	23.1 ± 5.87^a
SE	$29.4 \pm 6.18^{a,b}$	30.8 ± 7.03^b	$29.2 \pm 3.98^{a,b}$

Mean values with the same superscripts are not significantly different ($p > 0.05$).

MP, Scotchbond Multipurpose; SB, Single Bond; SE, Clearfil SE Bond

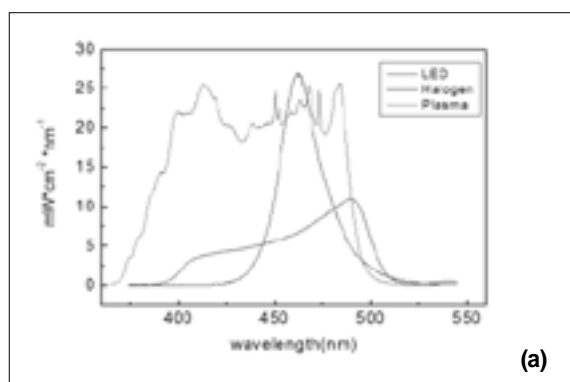


Figure 2(a). Spectral distributions of PAC, QTH and LED LCUs. PAC shows a broad spectral distribution with multiple peaks and QTH also has a broad spectrum but its peak (490 nm) deviated a little toward the lower end of IR range whereas LED shows a narrow spectral distribution around its peak at 462 nm.

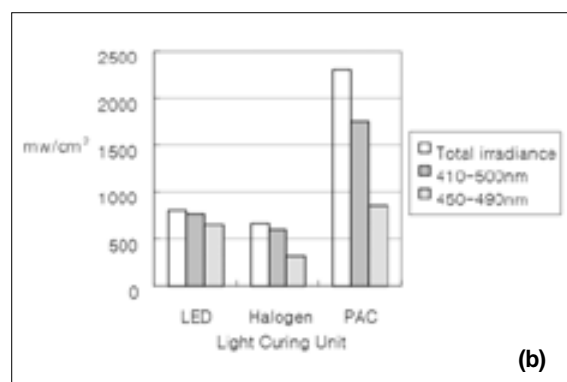


Figure 2(b). Total irradiance and irradiances in 450 - 490 nm and 410 - 500 nm regions. Power density of PAC is reduced to 76% and 37% of total intensity in 410 - 500 nm and in 450 - 490 nm region, respectively and that of QTH is reduced to 88% and 48% whereas that of LED is reduced to 96% and 81%.

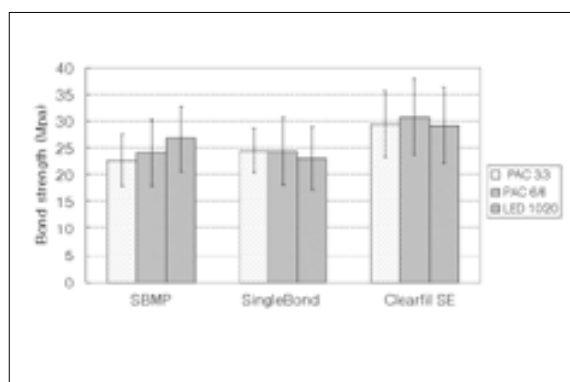


Figure 3. Mean shear bond strengths of DBAs cured with PAC and LED. There are statistically significant differences in the mean value among the different DBAs ($p < 0.001$) but not among the different LCUs ($P > 0.05$). There is no significant interaction between DBA and LCU.

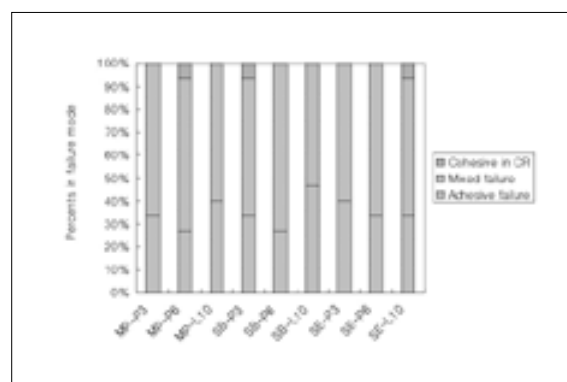


Figure 4. Failure modes. Mixed failure was the most predominant failure mode followed by adhesive failure. There were only 3 cases of composite cohesive failures and no extensive dentin cohesive failure. There was no significant difference among the 9 groups assigned. MP, Scotchbond Multipurpose; SB, Single Bond; SE, Clearfil SE Bond; P3, Curing with PAC for 3 seconds; P6, Curing with PAC for 6 seconds; L10, Curing with LED for 10 seconds.

IV. DISCUSSION

There were some differences in measurements among those reported by manufacturers, read by hand-held radiometers and obtained by EPM 1000 as shown in Table 3. According to the measurements

obtained by EPM 1000, the total irradiance of Apollo 95E was 2307 mW/cm² which is 2.86 times higher than 805 mW/cm² of Elipar FreeLight 2 and 3.42 times higher than 674 mW/cm² of VIP Junior. The irradiances of Apollo 95E in the range of 410 - 500 nm and 450 - 490 nm were still higher than those of Elipar

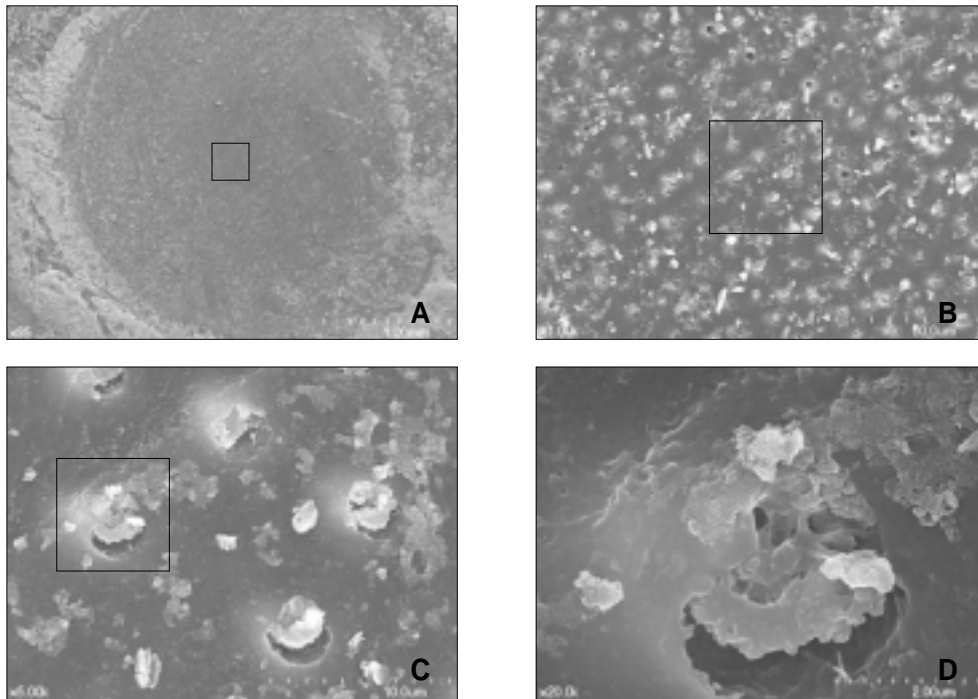


Figure 5(a). Adhesive failure (Clearfil SE Bond/Clearfil AP-X, SE cured with PAC for 6 seconds and AP-X was cured with PAC with 6 seconds). A, Gross shape of the fractured surface ($\times 35$); B, Higher magnification of marked area in a ($\times 1000$); C, Higher magnification of marked area in b ($\times 5000$), dentinal tubules and resin tags can be observed.; D, Higher magnification of marked area in c ($\times 20000$)

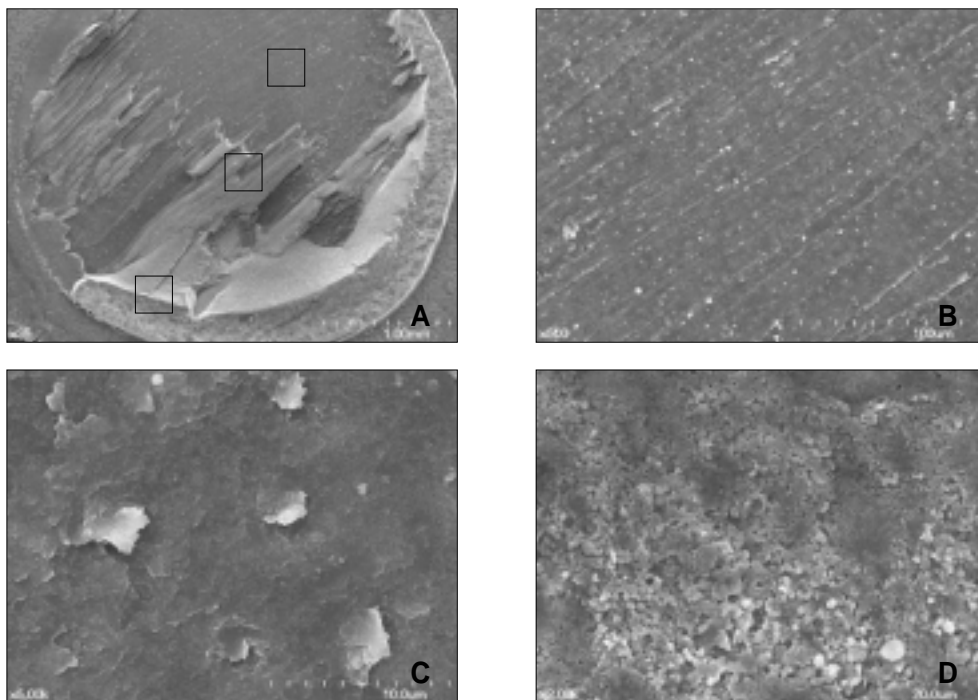


Figure 5(b). Mixed failure (Single Bond/Filtek Z250, SB was cured with PAC for 3 seconds and Z250 was cured with PAC for 3 seconds). A, Gross shape of the fractured surface ($\times 35$); B, Higher magnification of upper marked area of adhesive failure ($\times 500$); C, Higher magnification of middle marked area of mixed failure ($\times 5000$), mixture of adhesive and composite can be observed.; D, Higher magnification of lower marked area of composite cohesive failure ($\times 20000$), filler particles can be observed indicating presence of composite.

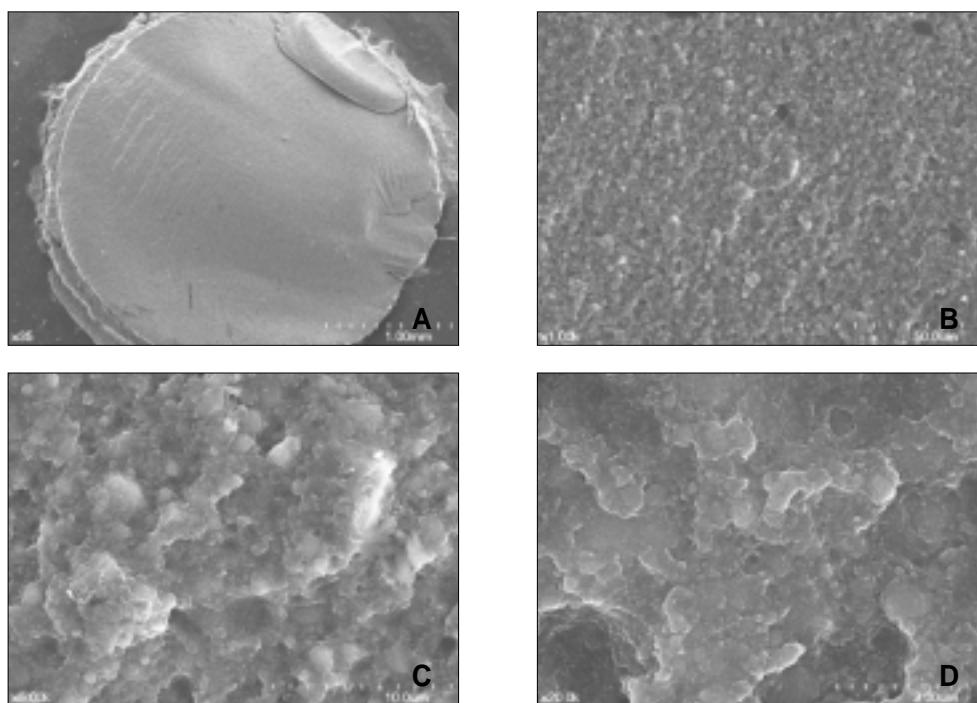


Figure 5(c). Cohesive failure in composite (ScotchBond MP/Filtek Z250, MP was cured with PAC for 6 seconds and Z250 was cured with PAC for 6 seconds). A, Gross shape of the fractured surface ($\times 35$); B, C, D, higher magnifications ($\times 1000$, $\times 5000$ and $\times 20000$) of surfaces with composite cohesive failure.

FreeLight 2 and VIP Junior in the respective regions even though the differences were smaller compared to those in total irradiance. LED is generally accepted to be wavelength efficient because it produces a narrower spectrum in an approximate wavelength range of 450 – 490 nm, delivering the greatest irradiance centered on a wavelength of approximately 470 nm which is close to absorption peak of camphorquinone^{3,10}. However, since camphorquinone (most commonly used photoinitiators) has maximum absorbance at 470 nm but shows a somewhat broader absorption spectrum (400 – 500 nm) than a typical LED emission spectrum^{11,12}, QTH curing may be more advantageous by allowing additional curing from wavelengths not present in LED units¹². PAC may also have the advantage of curing photoinitiators other than camphorquinone since it shows a broad emission spectrum comparable to that of QTH. It is not yet fully understood what is the optimum wavelength range of the curing lights.

The shear bond strength test results in this study

showed that light curing DBAs with either PAC for 3 seconds, PAC for 6 seconds or LED for 10 seconds did not make significant differences ($P > 0.05$). It was expected that the shear bond strength of DBAs cured with PAC for 3 seconds would be lower than those of DBAs cured with either PAC for 6 seconds or LED for 10 seconds because curing with PAC for 3 seconds produces the lowest energy density and because several studies^{13,14} reported that curing resin products with PAC for short time such as 3 seconds could produce improper cure. However, this study showed that even 3 second cure with PAC produced similar shear bond strength compared with LED for 10 seconds. The possible negative effect from polymerization shrinkage stress resulting from fast curing of PAC has been raised by some authors^{13,14}. In this study the thickness of DBAs applied is thin enough and shrinkage stress could have been directed to bonded dentin surface thus minimizing negative effect to bond strength. The composite placed on top of DBA bonded to dentin was also not more than 1.5

mm thick, which the light from LCUs could penetrate without losing much effectiveness.

The optimum curing time and energy density to properly cure resin based products is not clearly established yet. Recently, Lindberg *et al.*^{15,16)} reported that for resin composite, the exposure time per 2 mm increment may be reduced from 60 seconds to 20 seconds, and that with a 40 second exposure time, the increment thickness can be increased to 3.5 mm. With the advancements in light curing units and resin formulations including photoinitiators, it may be the right time to set a new standard for optimal curing time and energy density. Based on the shear bond strength test results of this study, it may be possible that as long as the energy density is above certain level, the increase of curing time does not substantially affect physical properties of cured resin products such as bond strength and that curing some resin based products including dentin bonding agents with PAC lights for 3 seconds is acceptable if careful precautions such as incremental layering not more than 1.5 mm are strictly followed.

SE Bond showed the highest shear bond strength in all three curing modes. However, it should be noted that all three DBAs used in this study showed shear bond strength more than 20 MPa which is considered clinically acceptable.

Although shear bond strength test method has been criticized for its uneven stress distribution and frequent dentin pull-out¹⁷⁻²⁰⁾, the popularity of this widely used test method remains unchanged owing to its relative simplicity²⁰⁾. In this test, modified chisel-on-iris method has been employed to produce reproducible results and minimize dentin pull-out as reported by Dickens and Milos²¹⁾. Applying true shear force in shear test may not be possible. However, the "chisel-on-iris supported with the Teflon wall" design employed in this study seemed to be effective because it did produce reproducible results and no extensive dentin pull-out.

V. CONCLUSION

The shear bond strength test results in this study showed that light curing DBAs with either PAC for 3

seconds, PAC for 6 seconds or LED for 10 seconds did not make significant differences ($P > 0.05$).

Further studies on mechanical properties and clinical performance of DBAs cured with PAC light will be needed to determine minimum exposure time and proper curing method specifically with PAC lights.

REFERENCES

1. Craig RG, Powers JM. Restorative dental materials. 11th Ed, 2001.
2. Althoff F, Hartung M. Advances in light curing. *Am J Dent* 13:77D-81D, 2000.
3. Jandt KD, Mills RW, Blackwell GB, Ashworth SH. Depth of cure and compressive strength of dental composites cured with blue light emitting diode (LEDs). *Dent Mater* 16:41-47, 2000.
4. Mills RW. Blue light emitting diodes - another method of light curing? *Br Dent J* 178:169, Letter 1995.
5. Stahl F, Ashworth SH, Jandt KD, Mills RW. Light-emitting diode (LED) polymerisation of dental composites: flexural properties and polymerisation potential. *Biomaterials* 21:1379-1385, 2000.
6. Price RBT, Felix CA, Andreou P. Evaluation of a dual peak third generation LED curing light. *Compendium* 26:331-348, 2005.
7. Kim SY, Lee IB, Cho BY, Son HH, Um CM. Curing effectiveness of a light emitting diode on dentin bonding agents. *J Biomed Mater Res Part B* 77B:164-170, 2006.
8. Caughman WF, Rueggeberg FA. Shedding new light on composite polymerization. *Oper dent* 27:636-638, 2002.
9. Christensen GJ. The light-curing mania. *JADA* 135:461-463, 2004.
10. Uhl A, Mills RW, Jandt KD. Polymerization and light-induced heat of dental composites cured with LED and halogen technology. *Biomaterials* 24:1809-1820, 2003.
11. Teshmia W, Nomura Y, Tanaka N, Urabe H, Okazaki M, Nahara Y. ESR study of camphorquinone/amine photoinitiator systems using blue-light emitting diodes. *Biomaterials* 24:2097-2103, 2003.
12. Ramp LC, Broome JC, Ramp MH. Hardness and wear resistance of two resin composites cured with equivalent radiant exposure from a low irradiance LED and QTH light-curing units. *Am J Dent* 19:31-36, 2006.
13. Peutzfeldt A, Sahafi A, Asmussen E. Characterization of resin composites polymerized with plasma arc curing units. *Dent Mater* 16(5):330-336, 2000.
14. Park SH, Krejci I, Lutz F. Microhardness of resin composites polymerized by plasma arc or conventional visible light curing. *Oper Dent* 27: 30-37, 2002.
15. Lindberg A, Peutzfeldt A, Dijken JWV. Effect of power density of curing unit, exposure duration, and light guide distance on composite depth of cure. *Clin Oral Invest* 9:71-76, 2005.
16. Lindberg A, Peutzfeldt A, Dijken JWV. Curing depths of a universal hybrid and a flowable resin composite cured with quartz tungsten halogen and light-emitting diode units. *Acta Odontol Scand* 62:97-101, 2004.

17. Sudsangiam S, Van Noort R. Do dentin bond strength tests serve a useful purpose? *J Adhes Dent* 1:57-67, 1999.
18. Van Noort R, Cardew GE, Howard IC. A study of the interfacial shear and tensile stresses in a restored molar tooth. *J Dent* 16:286-293, 1988.
19. Van Noort R, Noroozi S, Howard IC, Cardew G. A critique of bond strength measurements. *J Dent* 17:61-67, 1989.
20. Versluis A, Tantbirojin, Douglas WH. Why do shear bond tests pull out dentin? *J Dent Res* 76:1298-1307, 1997.
21. Dickens SH, Milos MF. Relationship of dentin shear bond strengths to different laboratory test designs. *Am J Dent* 15:185-192, 2002.

국문초록

전단접착강도와 관련된 Plasma Arc Curing Light의 중합효율평가

권영철 · 김선영 · 정세준 · 한영철 · 이인복 · 손호현 · 엄정문 · 조병훈*

서울대학교 치의학전문대학원 보존학교실

광물리학적 특성 분석을 위해 Apollo 95E (DMT Systems, Orange, CA; PAC 광중합기), Elipar Freelight 2 (3M ESPE, MN, USA; LED 광중합기) 그리고 VIP Junior (Bisco, Schaumburg, IL, USA; QTH 광중합기), 3종의 광중합기의 총광강도(Total intensity)와 spectral distribution을 측정하였고 특정 파장에 해당되는 광강도(Energy density)를 분석하였다. 상아질 전단접착강도의 측정을 위해 Scotchbond Multipurpose (3M ESPE), Single bond (3M ESPE) 그리고 Clearfil SE bond (Kuraray)가 사용되었다.

Plasma Arc Curing light (Apollo 95E) 광중합기는 여러개의 최대정점을 가지며 넓은 spectral distribution과 2307 mW/cm^2 의 높은 광강도를 나타내었고, VIP Junior 광중합기는 490 nm 에서 최대정점을 갖는 넓은 spectral distribution을 나타내었고, Elipar Freelight 2 광중합기는 462 nm 의 최대정점 주위로 좁은 spectral distribution을 보였다. Two-Way ANOVA와 Bonferroni's multiple comparison test를 이용하여 상아질 전단접착강도를 분석한 결과, PAC 광중합기와 LED 광중합기 간에 유의성 있는 차이를 보이지 않았으며 ($P > 0.05$), 상아질 접착제와 광중합기의 교호관계에도 유의성이 없었다. 그러나 상아질 접착제는 상호간에 유의성 있는 차이를 보였다 ($P < 0.001$).

주요어: PAC 광중합기, LED 광중합기, 상아질 접착제, 상아질 전단접착강도, Spectral irradiance, Energy density