

The Optimal Parameter for Radiation Dose in Pediatric Low Dose Abdominal CT: Cross-sectional Dimensions versus Body Weight¹

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Purpose: To investigate the best parameter between cross-sectional dimensions and body weight in pediatric low dose abdominal CT.

Materials and Methods: One hundred and thirty six children consecutively underwent weight-based abdominal CT. The subjects consisted of group 1 (79 children, weight range 10.0 - 19.9 kg) and group 2 (57 children, weight range 20.0 - 39.9 kg). Abdominal cross-sectional dimensions including circumference, area, anteroposterior diameters and transverse diameters were calculated. Image noise (standard deviation of CT density) was measured by placing a region of interest in the posterior segment of the right hepatic lobe on a CT image at the celiac axis. The measured image noise was correlated with the cross-sectional abdominal dimensions and body weight for subjects in each group.

Results: In group 1 subjects, area, circumference, transverse diameter, anteroposterior diameter, and body weight showed a significant positive correlation with image noise in descending order ($r = 0.63, 0.62, 0.61, 0.51, \text{ and } 0.49; p < 0.0001$). In group 2 subjects, transverse diameter, circumference, area, anteroposterior diameter, and body weight showed a significant positive correlation with image noise in descending order ($r = 0.83, 0.82, 0.78, 0.71, \text{ and } 0.71; p < 0.0001$).

Conclusion: Cross-sectional dimensions such as area, circumference, and transverse diameter showed a higher positive correlation with image noise than body weight for pediatric low dose abdominal CT.

Index words : Children

Abdomen, CT

Computed tomography (CT), radiation exposure

Computed tomography (CT), quality assurance

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Imaging parameters in pediatric CT should be minimized to the level of diagnostic quality as children have greater radiosensitivity, are exposed to a greater mean radiation dose due to the small size of the body, and children have a longer life expectancy than adults (1 - 5). Among strategies to minimize CT imaging parameters, setting up a body size-adaptive CT protocol is the first step. Body weight is the most commonly used body size parameter in determining the imaging parameters in pediatric CT. Initial attempts have been made by adjusting mA at a fixed potential of 120 or 140 kV (6, 7) and have been followed by reducing kV for lighter patients (8, 9). We also have used a weight-based pediatric CT protocol since 2000.

Theoretically, body weight may not be an optimal parameter for maintaining uniform CT image noise in patients with the same body weight but a different body habitus. In this respect, cross-sectional dimensions may be better than body weight for the determination of imaging parameters in pediatric CT. In adults, a few studies describing the relationship between cross-sectional dimensions and CT image noise have been reported (10 - 13). However, to the best of our knowledge an evaluation has not been conducted in children despite the issue that the CT radiation dose is critical in children and the body sizes of children are much more variable than body sizes of adults. Therefore, the aim of this study was to investigate the best parameter among the use of cross-sectional dimensions and body weight that showed the best correlation with image noise on pediatric abdominal low dose CT.

Materials and Methods

We retrospectively reviewed 186 consecutive abdominal CT studies in children weighing 10.0 - 39.9 kg that were performed between April 2004 and December 2004. The institutional review board approved the study and informed consents was not needed for the study. Among six body weight groups, only two body weight groups (group 1: 10.0 - 19.9 kg in body weight; group 2: 20.0 - 39.9 kg in body weight) were included in this study as the number of patients in the other groups was not sufficient for statistical analysis. Abdominal CT was performed with a four-slice CT scanner (Lightspeed QX/i; General Electric Medical Systems, Milwaukee, WI U.S.A.) according to a weight-based CT protocol (100 kV and 120 mA for group 1, 100 kV and 140 mA for group 2) in our institution. A four-slice spiral scan was

obtained with 0.5-sec gantry rotation time, 3.75-mm collimation, 3.75-mm slice thickness, and beam pitch 1.5. We excluded 50 of 186 abdominal CT examinations in the two groups when the body weight within one month before or after the examination date was not available, a patient was status post right hepatectomy, or lesions occupied the right lobe of the liver. Therefore, 136 abdominal CT examinations were included in this study: 79 studies in group 1 (mean age 3.1 years, M:F = 54:25) and 57 studies in group 2 (mean age 8.6 years, M:F = 33:24).

Body weight was obtained from the medical records of the patients. The mean interval between the CT examination and weight measurement was 6.3 days (range: 0 - 27 days) in group 1 and 6.3 days (range: 0 - 29 days) in group 2. Abdominal cross-sectional dimensions, including area, anteroposterior diameter, and transverse diameter, were measured on a CT image at the celiac axis. Abdominal circumference was estimated from the measured anteroposterior and transverse diameters. Image noise (standard deviation of CT density) was measured three times and was averaged by placing a rectangular region of interest ($1.3 \pm 0.6 \text{ cm}^2$) in the posterior segment of the right hepatic lobe with special attention not to include the hepatic vessels on the same CT image at the celiac axis (Fig. 1).

We evaluated whether cross-sectional dimensions, body weight, and image noise showed a normal probability curve. Image noise was correlated with abdominal cross-sectional dimensions and body weight for each group by the use of statistical software (MedCalc,

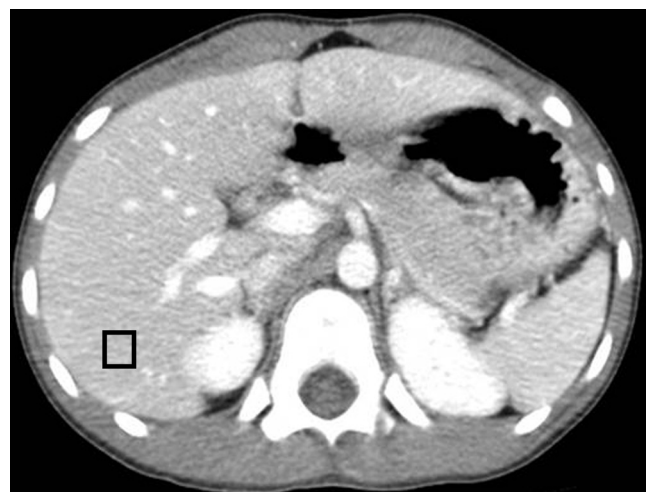


Fig. 1. An abdominal CT image at the level of the celiac axis shows a rectangular region of interest in the posterior segment of the right hepatic lobe used for measuring image noise (standard deviation of measured CT density).

Mariakerke, Belgium). A p -value of less than 0.05 was considered to indicate a statistically significant difference. Correlation coefficients (r) were considered as weakly positive correlation for $0.1 < r < 0.3$; strongly positive correlation for $0.3 < r < 0.7$; perfectly positive correlation for $0.7 < r < 1.0$.

Results

All data including abdominal cross-sectional dimensions, body weight, and image noise showed a normal probability curve. Abdominal cross-sectional dimensions and body weight in the two groups are described in Table 1. Measured image noise was 14.1 ± 2.1 in group 1 and 18.9 ± 3.9 in group 2. In group 1 subjects, area, circumference, transverse diameter, anteroposterior diameter, and body weight (in descending order) showed a strongly positive correlation ($r = 0.63, 0.62, 0.61, 0.51$ and 0.49 ; $p < 0.0001$) with image noise (Fig. 2). In group 2, a perfectly positive correlation was found between transverse diameter, circumference, area, anteroposterior diameter, and body weight (in descending order) and image noise ($r = 0.83, 0.82, 0.78, 0.71$ and 0.71 ; $p < 0.0001$) (Fig. 3). In both groups, body weight showed the lowest positive correlation with image noise and anteroposterior diameter showed the lowest or second lowest positive correlation with image noise. In contrast, area, circumference, and transverse diameter showed a higher positive correlation with image noise than the two body size parameters.

Discussion

In this study, we found that abdominal cross-sectional dimensions such as area, circumference, and transverse diameter showed a higher positive correlation with image noise of pediatric low dose abdominal CT than with body weight. Therefore, our results suggest that CT parameters based on abdominal cross-sectional dimensions may result in homogeneous noise of abdominal CT regardless of the body habitus of children. A strategy

based on these findings may have important practical advantages regarding both image quality and radiation dose issues over the use of a conventional weight-based strategy. With the use of a cross-sectional dimension-based protocol, non-diagnostic CT examinations in obese patients can be avoided. An unnecessarily high CT dose would not be used in slim patients.

Adjustment of CT parameters according to patient diameters has been reported to provide constant image noise in adults (10 - 13). Kalra et al. (11) correlated patient weight and cross-sectional dimensions with subjective image quality at standard dose abdominal CT and found that the transverse diameter of the abdomen had the strongest correlation with image quality. These results are similar to our results. However, these investigators used variable tube currents of abdominal CT and evaluated subjective image quality. On the contrary, we used the same tube current for each body weight group and measured image noise as one of objective evaluation methods for image quality. In addition, we could not find a single parameter that showed a consistent strong correlation with image noise, unlike the results of Karla and colleagues. In group 2 subjects (20.0 - 39.9 kg in body weight) that may have ellipsoid cross-sectional geometry similar to adults, the transverse diameter showed the strongest positive correlation with image noise, whereas area showed the strongest positive correlation with image noise in group 1 subjects (10.0 - 19.9 kg in body weight). This difference in correlation may be explained by differences in cross-sectional geometry between the subjects in the two groups: group 1 patients may have a more round cross-sectional geometry than in group 2 patients.

Measured image noise can be used to determine the diagnostic quality of a scanned CT image and ultimately allows one to decide appropriate body size adaptive CT parameters for each anatomic region. Other investigators also found that measurements of image noise could be used to adjust chest and abdominopelvic CT techniques for pediatric populations (14). The required image noise may be quite different for the purpose of a CT

Table 1. Abdominal Cross-sectional Dimensions and Body Weight in Groups 1 and 2

	APD (cm)	TD (cm)	AC (cm)	Area (cm ²)	Weight (kg)
Group 1	13.3 ± 1.0	18.5 ± 1.0	50.6 ± 2.8	206.9 ± 22.7	14.4 ± 2.5
Group 2	15.9 ± 1.9	22.3 ± 1.9	61.0 ± 5.9	300.2 ± 62.2	29.5 ± 5.2

Note. Group 1: 10.0 - 19.9 kg in body weight; Group 2: 20.0 kg-39.9 kg in body weight; APD: anteroposterior diameter; TD: transverse diameter; AC: abdominal circumference

All the numbers in the table represent mean \pm standard deviation.

study as well as for the scanned anatomic region. Therefore, it would be very helpful to determine optimal CT parameters for a CT study when the required level of image noise was already well established.

Further studies are necessary to determine the required image noises of various CT studies; such studies have seldom been performed. Subsequently, one can formulate an equation for CT parameters according to cross-

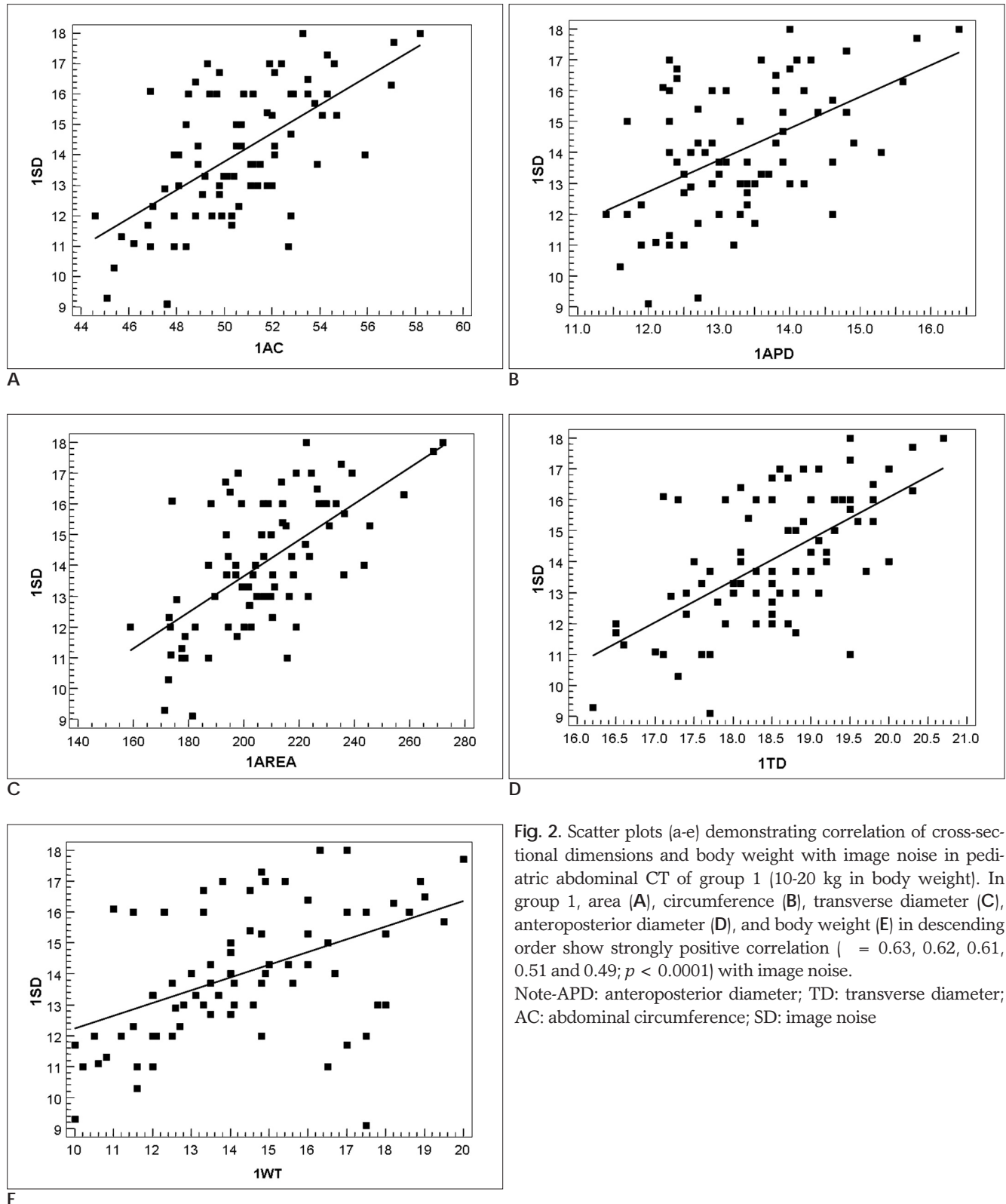


Fig. 2. Scatter plots (a-e) demonstrating correlation of cross-sectional dimensions and body weight with image noise in pediatric abdominal CT of group 1 (10-20 kg in body weight). In group 1, area (A), circumference (B), transverse diameter (C), anteroposterior diameter (D), and body weight (E) in descending order show strongly positive correlation ($r = 0.63, 0.62, 0.61, 0.51$ and 0.49 ; $p < 0.0001$) with image noise. Note-APD: anteroposterior diameter; TD: transverse diameter; AC: abdominal circumference; SD: image noise

sectional dimension and/or attenuation. By using such an equation, one could adjust CT parameters by an individual rather than by a group.

Body weight is globally used in determining CT para-

meters, as it is easy to obtain. A cross-sectional dimension should also be easy to obtain as a parameter to be used in clinical practice. In this regard, one should define a certain anatomic level for a CT study (for exam-

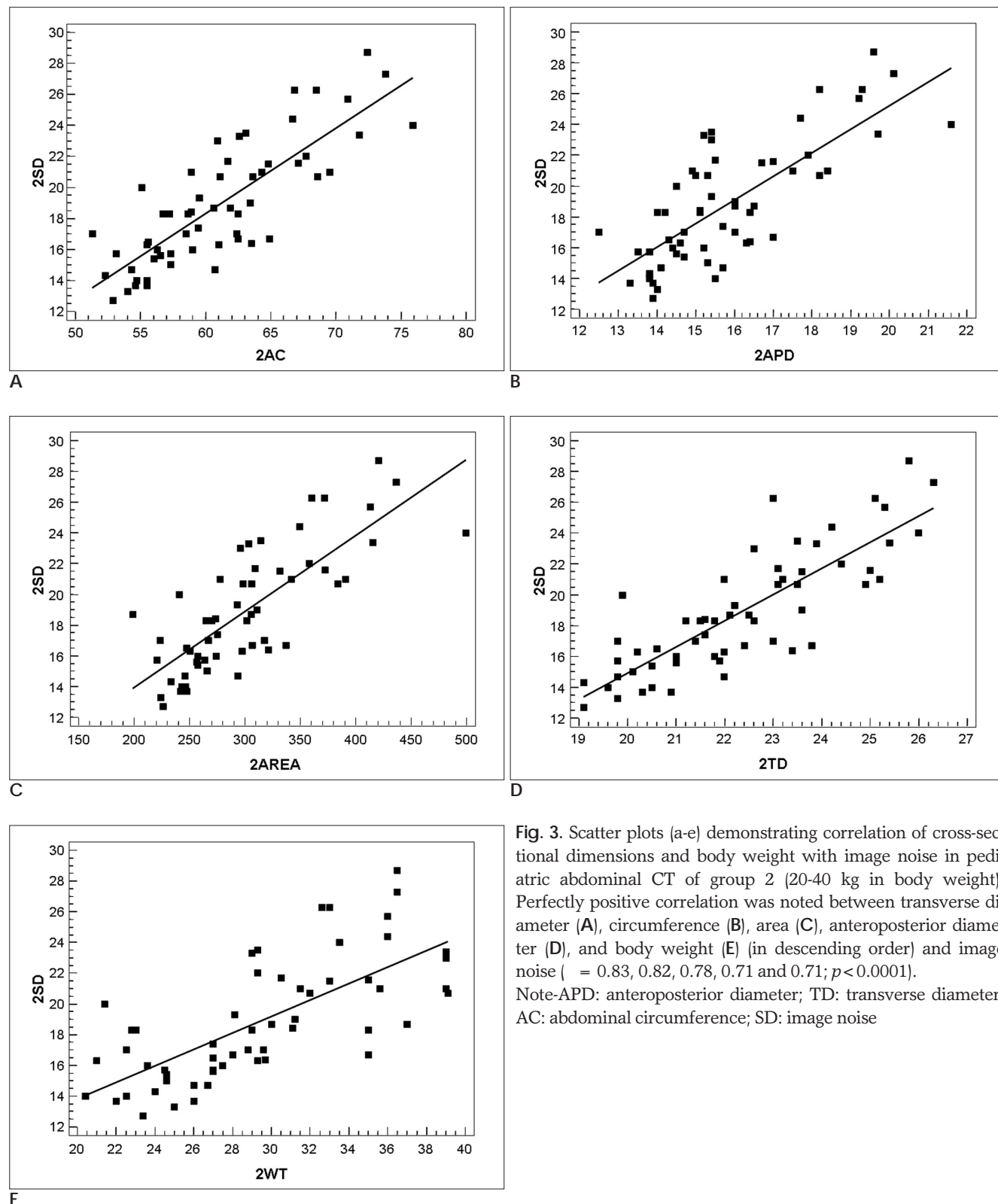


Fig. 3. Scatter plots (a-e) demonstrating correlation of cross-sectional dimensions and body weight with image noise in pediatric abdominal CT of group 2 (20-40 kg in body weight). Perfectly positive correlation was noted between transverse diameter (A), circumference (B), area (C), anteroposterior diameter (D), and body weight (E) (in descending order) and image noise ($r = 0.83, 0.82, 0.78, 0.71$ and 0.71 ; $p < 0.0001$). Note-APD: anteroposterior diameter; TD: transverse diameter; AC: abdominal circumference; SD: image noise

ple, the celiac axis level for abdominal CT) first. Next, the area and transverse diameter may be measured from a very low dose CT image at a predefined anatomic level. For that purpose, an image obtained for bolus tracking of contrast-enhanced CT can be used. Circumference can be directly measured at a predefined anatomic level by the use of a ruler before the CT examination.

In this study, the anteroposterior diameter had the lowest or the second lowest positive correlation with image noise. This finding is easily explained by the fact that in an ellipsoid cross-sectional geometry, CT image noise is principally influenced by the transverse diameter rather than by the anteroposterior diameter. Actually, this is a basic principle in angular tube current modulation, in which tube current in the anteroposterior direction can be reduced without a significant increase in image noise. Tube current modulation is a useful dose-reducing technique and it should be routinely used in pediatric CT if available (15). We did not apply the tube current modulation technique to pediatric abdominal CT as the CT system used in this study did not provide tube current modulation. Because image noise may be slightly affected by tube current modulation, a correlation study with image noise may actually be more accurate without tube current modulation than with tube current modulation.

In addition to body size parameters including cross-sectional dimensions and body weight, mean attenuation of CT images is another important factor for determining image noise. In an adult study, other investigators have suggested that a new topogram-based estimate containing a mean attenuation value might be better for individual CT dose adaptation than the use of other body size parameters (16). However, the method was too complex to be used in clinical practice. A study to find an optimal and practical way to determine CT parameters based on both cross-sectional parameter and attenuation value is ongoing in our department.

This study has several limitations. First, only two body weight groups (between 10 and 40 kg) were included as the number of CT examinations in the other groups was insufficient to be analyzed statistically. Thus, other body weight groups may not show the same results as the two body weight groups evaluated in this study. However, we believe that our results demonstrate a higher correlation of cross-sectional dimensions with image noise than with body weight in pediatric abdominal CT and demonstrate minor differences in cor-

relation strengths among the different body weight groups. Second, a small error from circumference estimation may be inevitable. However, direct measurement of circumference is virtually impossible on a CT image and we believe that such an error did not substantially affect our results.

In conclusion, cross-sectional dimensions such as area, circumference, and transverse diameter show a higher positive correlation with image noise than body weight for pediatric low dose abdominal CT. Therefore, pediatric CT based on such cross-sectional dimensions may result in more uniform image noise irrespective of body habitus than pediatric CT based on body weight.

References

1. Kalra MK, Maher MM, Toth TL, Hamberg LM, Blake MA, Shepard JA, et al. Strategies for CT radiation dose optimization. *Radiology* 2004;230:619-628
2. Lee CI, Haims AH, Monico EP, Brink JA, Forman HP. Diagnostic CT scans: assessment of patient, physician, and radiologist awareness of radiation dose and possible risks. *Radiology* 2004;231:393-398
3. McNitt-Gray MF. AAPM/RSNA physics tutorial for residents: topics in CT - radiation dose in CT. *Radiographics* 2002;22:1541-1553
4. Linton OW, Mettler FA Jr. National conference on dose reduction in CT, with an emphasis on pediatric patients. *AJR Am J Roentgenol* 2003;181:321-329
5. Goo HW. Pediatric CT: understanding of radiation dose and optimization of imaging techniques. *J Korean Radiol Soc* 2005;52:1-5
6. Donnelly LF, Emery KH, Brody AS. Minimizing radiation dose for pediatric body application of single detector helical CT: strategies at a large children's hospital. *AJR Am J Roentgenol* 2001;176:303-306
7. Frush DP, Soden B, Frush KS, Lowry C. Improved pediatric multi-detector body CT using a size-based color-coded format. *AJR Am J Roentgenol* 2002;178:721-726
8. Sigal-Cinqualbre AB, Hennequin R, Abada HT, Chen X, Paul JF. Low-kilovoltage multi-detector row chest CT in adults: feasibility and effect on image quality and iodine dose. *Radiology* 2004;231:169-174
9. Huda W, Scalzetti EM, Levin G. Technique factors and image quality as functions of patient weight at abdominal CT. *Radiology* 2000;217:430-435
10. Haaga JR, Miraldi F, Macintyre W, LiPuma JP, Bryan PJ, Wiesen E. The effect of mAs variation upon computed tomography image quality as evaluated by in vivo and in vitro studies. *Radiology* 1981;138:449-454
11. Kalra MK, Maher MM, Prasad SR, Hayat S, Blake MA, Varghese J, et al. Correlation of patient weight and cross-sectional dimensions with subjective image quality at standard dose abdominal CT. *Korean J Radiol* 2003;4:234-238
12. Starck G, Lonn L, Cederblad A, Forsell-Aronsson E, Sjostrom L, Alpsten M. A method to obtain the same level of CT image noise for patients of various sizes, to minimize radiation dose. *Br J Radiol* 2002;75:140-150
13. Wilting JE, Zwartkruis A, van Leeuwen MS, Timmer J, Kamphuis AG, Feldberg M. A rational approach to dose reduction in CT: in-

gated heart CT by combined tube current modulation. *Pediatr Radiol* 2006;36:344-351

16. Menke J. Comparison of different body size parameters for individual dose adaptation in body CT of adults. *Radiology* 2005;236: 565-571

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