

가
 (3D - MRI) 2
 (2D - MRI) 3D - MRI
 10 1.5 - T MRI
 3D - MRI Gd - DTPA (0.2 mmol/kg, 4 cc/sec) 10
 2D - MRI 3D - MRI
 paired Student t - test Bland - Altman . 60

kappa
 (p=0.11) (p=0.34) 가 Bland -
 Altman =0.674) (=0.615) 가 (가
 2D - MRI 가 가 3D - MRI
 MRI 가 가 가 3D -

(myocardial viability) 180 가
 가 (gadolinium) 가 0 가 (null point)
 (delayed hyperenhancement) MRI 가
 (1 - 5) FDG -
 PET (fluorodeoxyglucose - positron emission tomography) 가 MRI
 (6, 7). (transmural extent) (8, 9). MRI
 trueFISP (fast imaging with steady precession)
 turboFLASH (fast low angle shot)
 MRI 가 가
 (8). 2 MRI
 (1, 2). 가 가
 가 (4, 8 - 10). 10 - 15
 (inversion recovery pulse) T1 6 - 15
 wash - out 가
 (4, 10).

가 , 220 - 280 msec (field of view) 250 mm, (matrix) 192 x 192 .

(navigator - echo sequence) 10

4 . 2D - MRI IR - TFE .

3

MRI 178 msec . 220 -

(10). , 3D - MRI 350 msec . 320 mm, 304 x

2D - MRI 가 265 . 10 - 15

10 3D - MRI

가 3D - MRI 2D - 2D - MRI 9 .

MRI 3D - MRI .

가

3D - MRI 2D - MRI

2003 6 10 가

2D - MRI 3D - MRI 10

가 9 , 가 1

54 - 71 63.2 .

(ejection fraction) $34.8 \pm 10.1\%$.

MRI 16

(coronary artery bypass surgery) (blood pool)가

9

가 MRI .

(E) (N) (con -

trast - to - noise ratio, CNR) :

CNR= (SIE - SIN)/noise, SI=signal intensity. 10 - 30

cm²

(transmural

extent) (segmental width)

60 (6 x 10) .

Gd - DTPA (0.2 mmol/kg, 4 cc/sec)(Magnevist; Schering, Berlin, Germany)

(first - pass perfusion image)

10

3D - MRI 2D - MRI

Table 1 . 3D - MRI inversion recovery prepared turbofield echo (IR - TFE)

(column)

(dome) (acceptance window) 6 mm .

(acquisition window) 가 70

113 msec . (inversion time)

Table 1. MR Imaging Parameters

Parameter	3D-MRI	2D-MRI
Echo time (msec)	2.0	1.6
Repetition time(msec)	4.2	5.2
Flip angle (°)	15	15
Inversion time(msec)	220 - 280	220 - 350
Electrocardiography trigger	Every heartbeat	Every heartbeat
Number of phase encoding	192	265
Acquisition window (msec) [†]	113	178
Trigger delay (msec) [†]	654	654
Field of view (mm)	250	320
Matrix	192 x 192	304 x 265
Number of sections	10*	10*
Slice thickness(mm)	10	10
Gap (mm)	0	0
Number of averaging	2	3

*10 in nine patients and 9 in one patient.

[†] If, the heart rate of a patient is 70 per minute.

60 6 (, ,) (Fig. 1).
 9
 99 . 99
 (image blurring)
 가 14 3D - MRI 2D - MRI
 510 (6 × 85) .
 (transmural extent of hyperenhancement) 3
 : 0, (no hyperenhancement); 1,
 (no full transmural extent); 2,
 (full transmural extent).
 (segmental width of hyperenhancement) 3 : 0,
 (no hyperenhancement); 1, (partial
 segmental width of hyperenhancement); 2,
 (full segmental width of hyperenhancement) (Fig. 1).
 (apex), (middle), (base)
 2 - 3 . 3 ,

Paired Student t - test Bland - Altman

paired Student

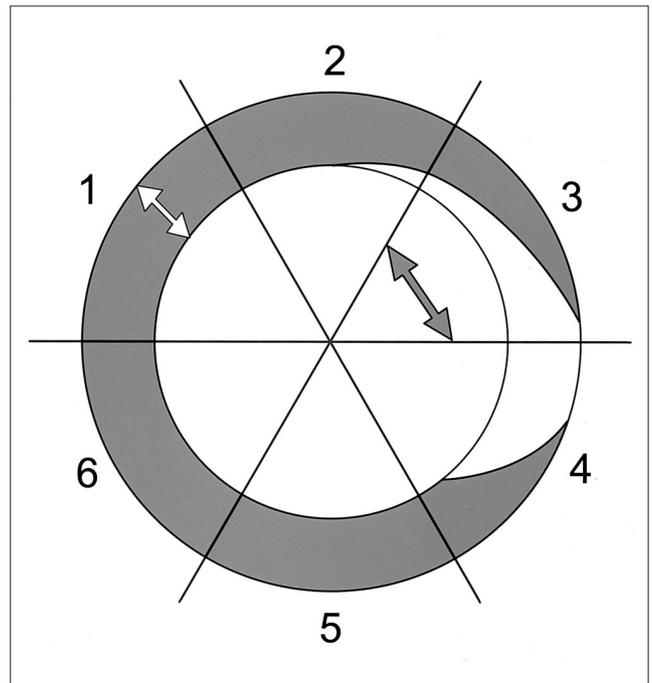
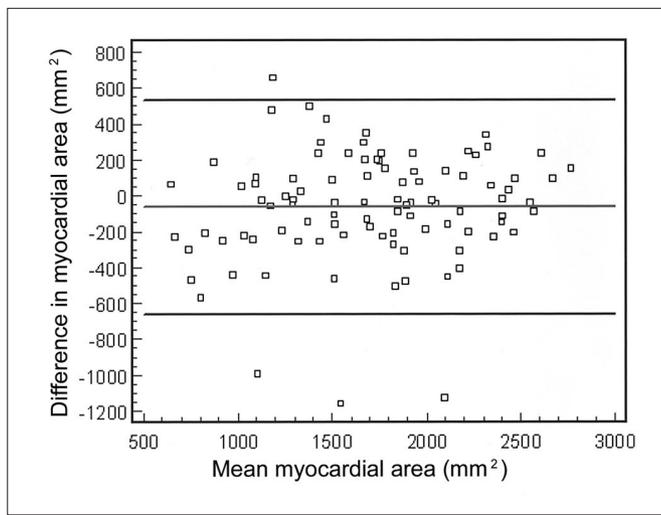
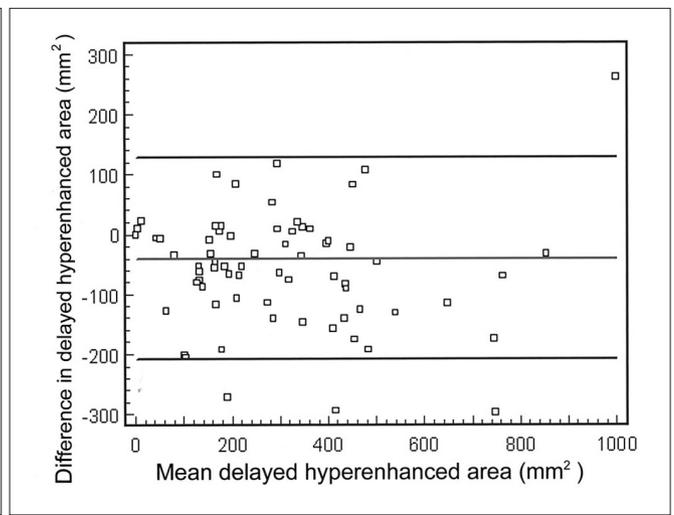


Fig. 1. Schematic shows 6-segment model and analysis of spatial extent of hyperenhancement. Gray zone: normal myocardium. White zone: hyperenhanced myocardium. Distribution of hyperenhancement throughout myocardial wall (transmural extent, white arrow) and width of segments (segmental width of hyperenhancement, gray arrow) were scored. Score for segment 2 is 1 (no full transmural extent and partial segmental width) in both transmural extent and segmental width. Score for segment 3 is 2 (full transmural extent and segmental width) in both transmural extent and segmental width. Score for segment 4 is 2 in transmural extent but is 1 in segmental width.



A
Fig. 2. Bland-Altman plots.



B. Delayed hyperenhanced areas on MR images obtained with 2 D and 3 D-MRI.

Findings reveal no relevant bias, with acceptable limits of agreement between the two sequences for the quantification of total myocardial areas and delayed hyperenhanced areas.

t - test
 (agreement) kappa
 : < 0.21, poor agreement; =0.21 - 0.40, fair; =0.41 - 0.60, moderate; =0.61 - 0.80, good; and > 0.80, excellent. P value 0.05

3D - MRI 2D - MRI (: 16.2 cm² ± 2.2
 16.8 cm² ± 2.2, p=0.1114) (: 1.9
 cm² ± 1.2 2.3 cm² ± 1.2, p=0.3434)
 . Bland - Altman (systemic
 difference) (: 0.65 cm²; 95%
 : - 6.61, +5.31 cm²) (:
 0.41 cm²; 95% : - 2.09, +1.28 cm²)
 ±5.97 cm², ±1.68 cm² (Fig. 2).
 (: 49.9 ± 29.6 49.1 ± 27.8, p=0.9355).
 (=0.615)

(=0.674) (good agreement)
 (Table 2). , ,
 (= : 0.672, : 0.648, :
 0.647) 가
 (= : 0.570, : 0.599, : 0.612) (Fig. 3).
 3 D - MRI 가 3D - MRI
 150

Table 2. Agreement between 2D-MRI and 3D-MRI for Spatial Extent of Hyperenhancement

Finding	Agreement	
	Common	95% CI
Transmural extent	0.615	0.553 - 0.677
Apical	0.570	0.457 - 0.684
Middle	0.599	0.494 - 0.704
Basal	0.612	0.491 - 0.733
Segmental width	0.674	0.617 - 0.730
Apical	0.672	0.570 - 0.775
Middle	0.648	0.553 - 0.743
Basal	0.647	0.532 - 0.761

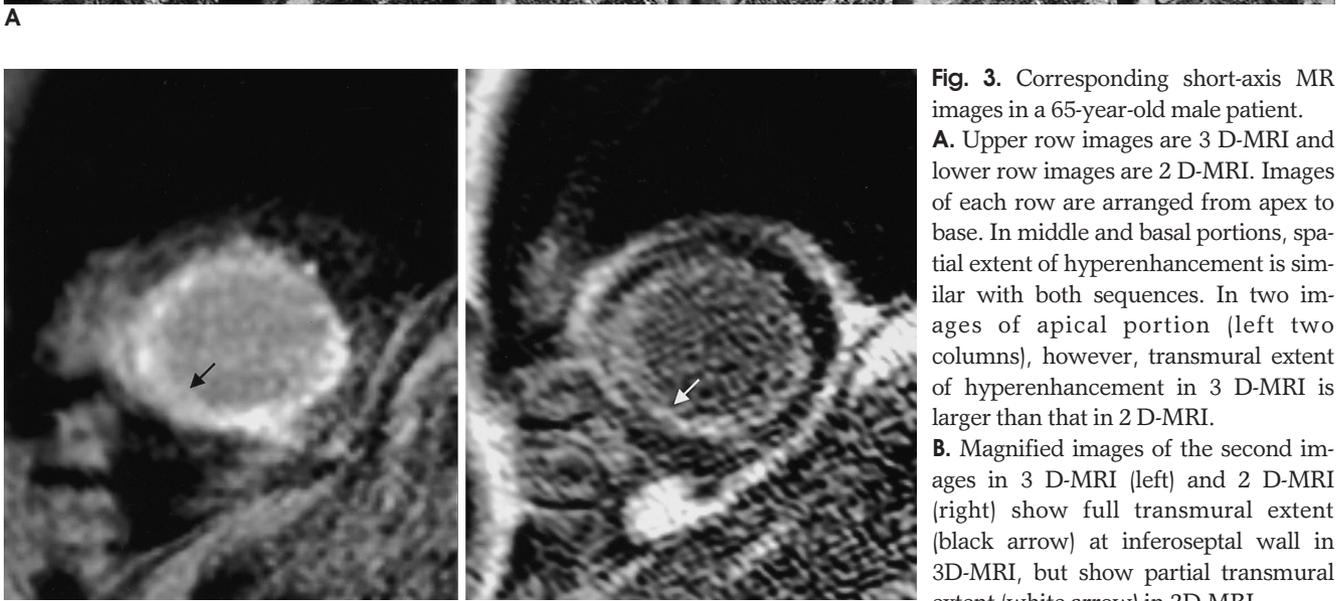
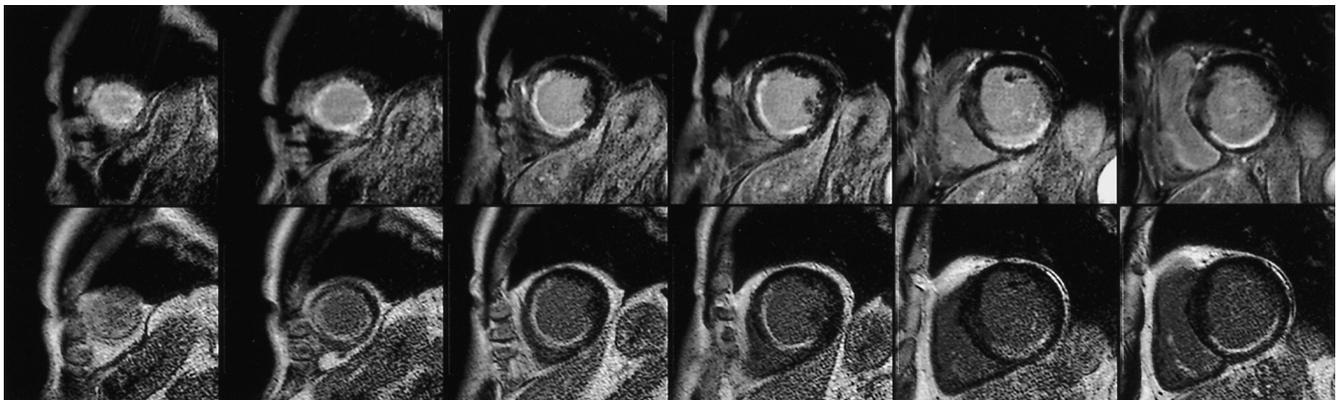


Fig. 3. Corresponding short-axis MR images in a 65-year-old male patient.
A. Upper row images are 3 D-MRI and lower row images are 2 D-MRI. Images of each row are arranged from apex to base. In middle and basal portions, spatial extent of hyperenhancement is similar with both sequences. In two images of apical portion (left two columns), however, transmural extent of hyperenhancement in 3 D-MRI is larger than that in 2 D-MRI.
B. Magnified images of the second images in 3 D-MRI (left) and 2 D-MRI (right) show full transmural extent (black arrow) at inferoseptal wall in 3D-MRI, but show partial transmural extent (white arrow) in 2D-MRI.

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Myocardial Viability: Comparison of Free-Breathing Navigator-echo-gated Three-Dimensional Inversion-Recovery Gradient-Echo MR and Standard Multiple Breath-Hold Two-Dimensional Inversion-Recovery Gradient-Echo MR¹

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Purpose: To compare a free-breathing, navigator-echo-gated, three-dimensional, inversion-recovery, gradient-echo, MR pulse sequence (3D-MRI) with standard, multiple breath-hold, two-dimensional, inversion-recovery, gradient-echo MR (2D-MRI) for the evaluation of delayed hyperenhancement of nonviable myocardium in patients with chronic ischemic heart disease.

Materials and Methods: Ten patients with chronic ischemic heart disease were enrolled in this study. MRI was performed on a 1.5-T system. 3D-MRI was obtained in the short axis plane at 10 minutes after the administration of Gd-DTPA (0.2 mmol/kg, 4 cc/sec). Prospective gating of the acquisition based on the navigator echo was applied. 2D-MRI was performed immediately after finishing 3D-MRI. The area of total and hyperenhanced myocardium measured on both image sets was compared with paired Student t-test and Bland-Altman method. By using a 60-segment model, the transmural extent and segmental width of the hyperenhanced area were recorded by 3-scale grading method. The agreement between the two sequences was evaluated with kappa statistics. We also evaluated the agreement of hyperenhancement among the three portions (apical, middle and basal portion) of the left ventricle with kappa statistics.

Results: The two sequences showed good agreement for the measured area of total and hyperenhanced myocardium on paired t-test ($p=0.11$ and $p=0.34$, respectively). No systematic bias was shown on Bland-Altman analysis. Good agreement was found for the segmental width ($\kappa=0.674$) and transmural extent ($\kappa=0.615$) of hyperenhancement on the segmented analysis. However, the agreement of the transmural extent of hyperenhancement in the apical segments was relatively poor compared with that in the middle or basal portions.

Conclusion: This study showed good agreement between 3D-MRI and 2D-MRI in evaluation of non-viable myocardium. Therefore, 3D-MRI may be useful in the assessment of myocardial viability in patients with dyspnea and children because it allows free-breathing during the examination.

Index words : Heart
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