

가: 가

VX2

1

2

: 가 VX2 (perfusion) (MRI)
 VX2 ,
 가 MRI
 : 가 12 , VX2 7 - 14
 MRI . MRI VX2
 ,
 ,
 , VX2 VIII
 , 가 VX2 (MVD)
 : VX2 15 1 - 3 cm .
 VX2 9 - 20
 , 12 - 50
 . VX2 13 - 16 (15)
 28 - 36 (32) ($p < 0.01$).
 VX2 27 - 84% (47%) , 36 - 82% (56%)
 . VX2 MVD 200
 75 17 ($p < 0.01$).
 : MRI 가 VX2
 . MRI ,

(magnetic resonance image, MRI
) 가 MRI가 가
 , (1, 2). (3, 4). MRI
 , MRI MRI(perfusion - weighted MRI)
 가
 (5, 6). MRI
 가

¹
²
 2000
 2001 1 8 2001 6 28
 - (blood brain barrier)
 (3, 4, 7 - 10). ,

| | | | | |
|--|--|-----------------------|--|--|
| | | | : | |
| | 가 | | | 가 |
| | (intravascular space) | | 1 mL | 18 |
| (extravascular space) | 가 | | (Medicut ;Jelcco, San Francisco, U.S.A.) | |
| MRI | 가 | MRI | (Cook, Bloomington, U.S.A.) | |
| 가 | . | echoplanar MRI | 0.1 mL | . |
| imaging (EPI) | 가 | (11 - 16), | | 가 |
| | 가 | MRI | MRI | |
| | , | , | | VX2 |
| | , , | | MRI | , VX2 |
| | | | | 7 - 14 |
| | 가 | | | |
| . Roncalli | (17) | | MRI | 가 |
| | 가 | | 가 | 23 |
| (low grade dysplastic nodule, regenerative nodule) | | | 가 | |
| | | | MRI | |
| | | | MRI | 1.5 T Signa Horizon Echospeed MRI scanner(General Electric Medical Systems, Milwaukee, WI, U.S.A.) . 가 |
| | | | | 5 |
| | | | (flat type GP surface coil) | |
| | | | MRI | MRI |
| | | | T1 | (T1 weighted image, T1WI) T2 |
| VX2 | 가 | | | (T2 weighted image, T2WI) |
| VX2 | | MRI | T1WI | (repetition time, TR)/ |
| | , | | | (time to echo, TE)=400 msec/9 msec , T2WI |
| | | 가 | TR/TE=3400 msec/98 msec | |
| | MRI | 가 | (field of view, FOV) 18×16 cm, | (acquisition matrix) 256×192, |
| | | | | (number of excitation) 2, |
| | | | | (slice thickness) 5 mm, |
| | | | | (intersection gap) 2.5 mm |
| | VX2 | | | 5 . T1WI, T2WI |
| | 2.5 - 3.5 kg (3.1 kg) 가 | | MRI | |
| 12 | . 가 | VX2 | MRI single-shot EPI | |
| | | VX2 | Single-shot EPI | MRI TR infi- |
| 가 (carrier rabbit) | potassium chloride (KCl) | | nite, TE 20 msec, bandwidth 2080 Hz/pixel, | 128 × |
| 5 mL | | | 128, | 4 mm, |
| | | | 1.5 mm, | 18 × 16 |
| | | | cm, | 1 |
| | | | 0.1 mmol/kg gadolinium - DTPA(Magnevist ; Schering, Berlin, Germany) | 2 - 3 mL/sec |
| | | | MRI | |
| | | | 120 | 2 |
| | | | | 60 |
| | 가 | | MRI | |
| , 5 mL DMEM/F-12 | (Gibco Laboratories, Life Technology Inc., Grand Island, New York, U.S.A.) | | | |
| | Xylazine hydrochloride | | MRI workstation(GE Advantage Windows | |
| (Rompun ; | , |) ketamine hydrochlo- | 2.0) | . 60 MRI |
| ride (Ketalar ; | , |) 1 : 1 | VX2 | (region |
| mL/kg | 가 | | of interest, ROI) | |
| | 가 | | | |

(%)=

× 100(%)

0%
, 0%

가 가

ROI

(200)

MRI 가 thiopental sodium(Pentothal ;
, ,) (90 mg/kg)

. VX2

10%

hematoxylin - eosin

(18), VIII

(microvessel density, MVD
(40)

가 가

MVD

MVD

MVD

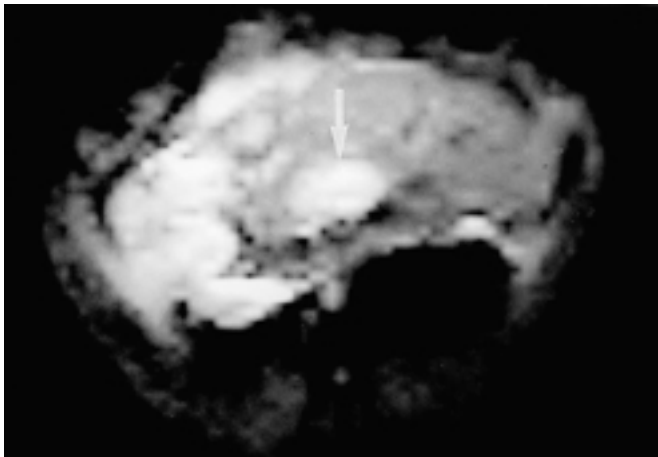
MVD

VX2

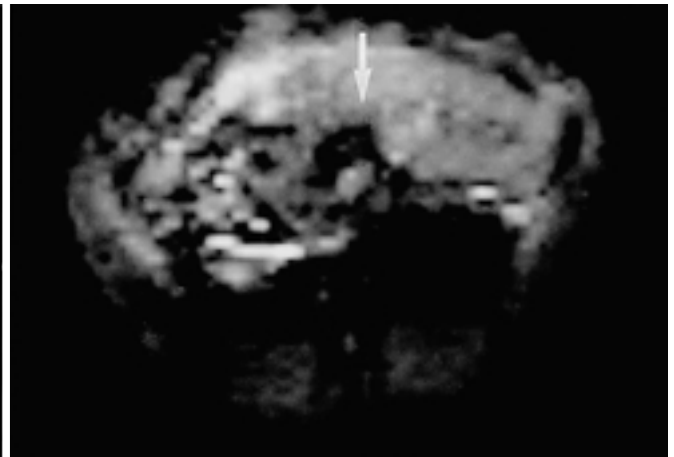
t - test

가

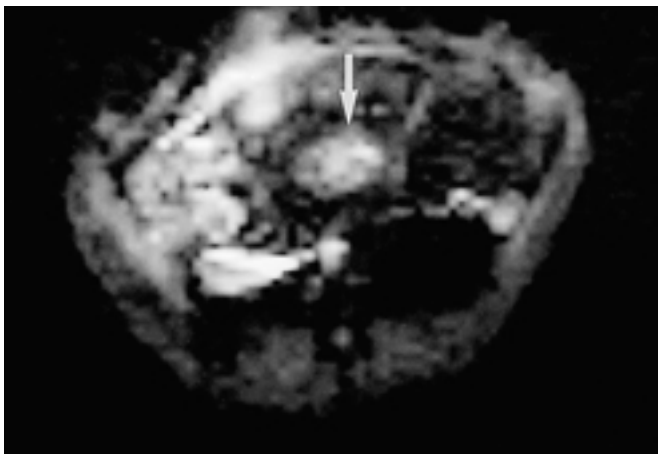
VX2



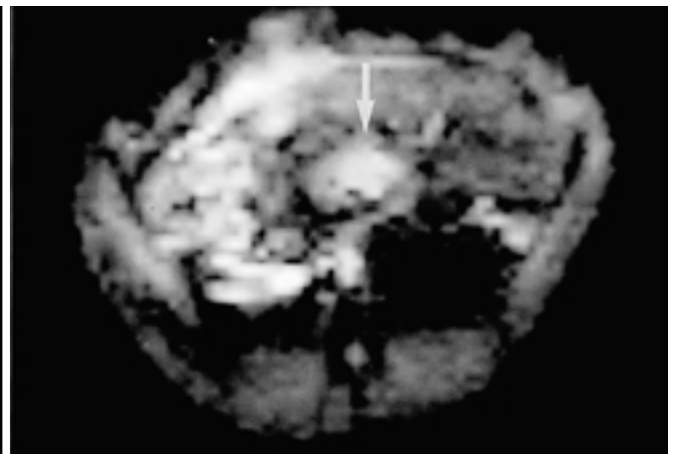
A



B



C



D

Fig. 1. Time-course perfusion MR images of a rabbit liver obtained before(A), 14 seconds(B), 32 seconds(C), and 120 seconds(D) after bolus injection of gadolinium-DTPA. The maximum signal intensity decrease of VX2 carcinoma[arrow] was observed at (B) and that of normal liver parenchyma was observed at (C).

t - test

MVD 가

12 가 15 VX2
1 - 3 cm 1.8 cm

MRI

VX2 MRI 가

VX2 MRI (Fig. 1).

VX2 9 - 20

12 - 50

(Fig. 2).

VX2 13 - 16 (15)

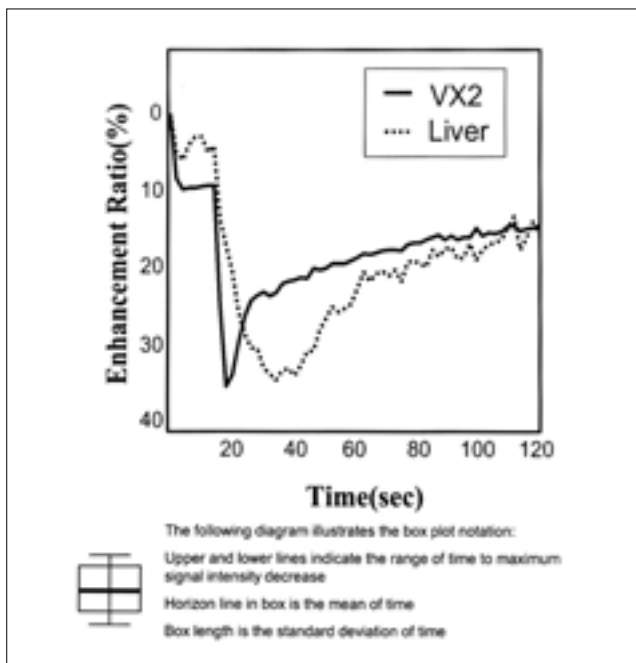


Fig. 2. Time-intensity perfusion curves of VX2 carcinoma(solid line) and normal liver parenchyma(dotted line). Perfusion curves demonstrate rapid decrement and immediate recovery of signal intensity of VX2 carcinoma at early perfusion phase and slower decrement and gradual recovery of that of normal liver parenchyma at late perfusion phase.

가

28 - 36 (

32) (Fig. 3),

가 ($p < 0.001$).

VX2

27 - 84%(47%) , 36 - 82%(

56%) (Fig. 4),

가 .

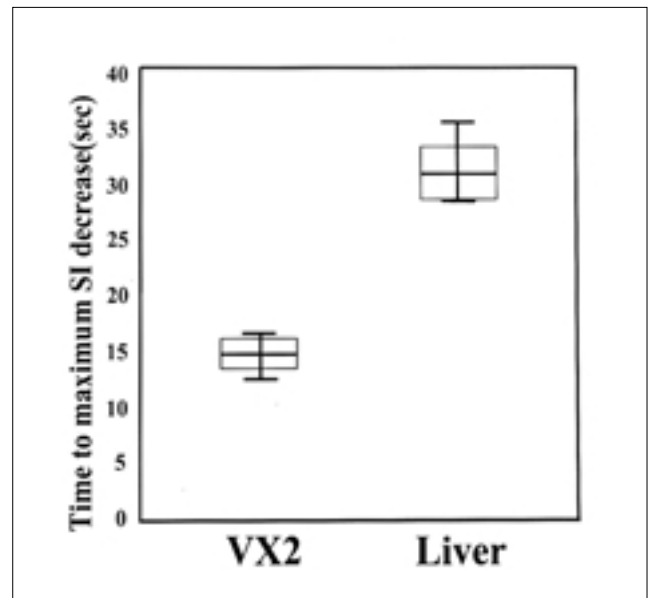


Fig. 3. Box plot demonstrates the ranges and means of time to maximum signal intensity(SI) decrease corresponding to VX2 carcinoma(n = 15) and normal liver parenchyma(n = 15).

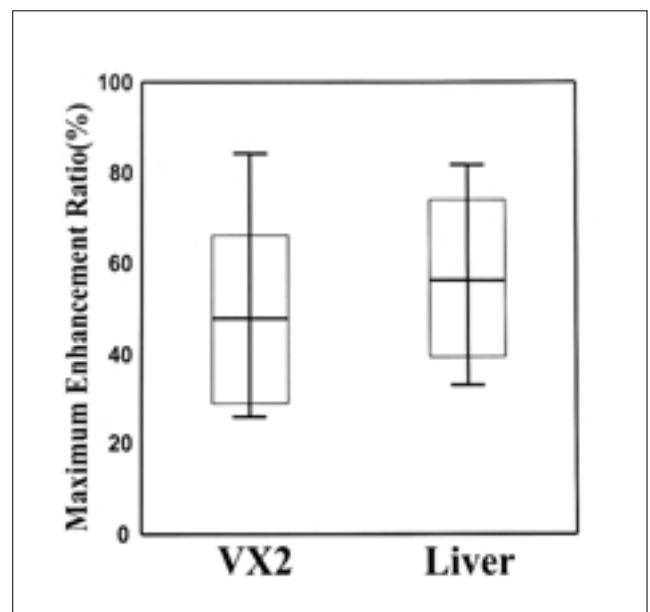


Fig. 4. Box plot demonstrates the ranges and means of maximum enhancement ratios corresponding to VX2 carcinoma(n = 15) and normal liver parenchyma(n = 15).

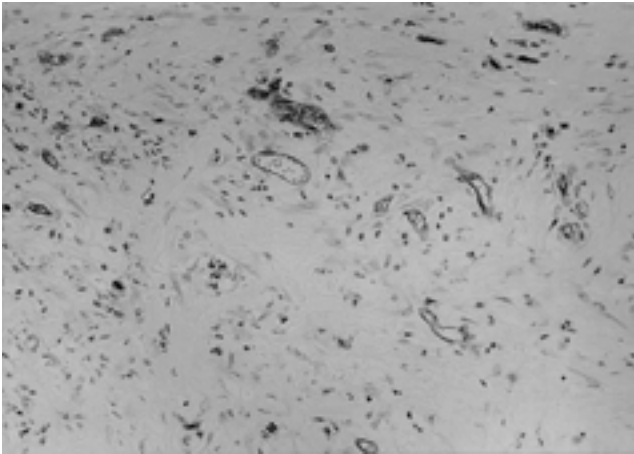


Fig. 5. Immunohistochemical stain for factor VIII-related antigen of the hepatic VX2 carcinoma shows rich neo-microvessels highlighted as brown colored slit-like structure (Factor VIII stain, $\times 200$).

VX2
가
가
(pyknosis), (karyolysis)
가
가
necrosis) . VX2
(coagulative
VX2
가
(Fig. 5). VX2
200 75 (62 - 95)
17 (10 - 24)
가 ($p < 0.001$).
(angiogenesis)
(18 - 22).
가
(computed tomography), MRI,
(23 - 25),
가
MRI

MRI 가
1800
(arterial spin - tagging) (3).
MRI MRI
MRI T2 T2*
(6). 가 T1
T2 T2 가
가 (target organ)
(local magnetic field inhomogeneity)
(phase coherence)
가
(4, 7). 가
T2 T2*
MRI T2*
(gradient echo imaging) (8, 11).
EPI 1 10 - 20
(extracellular contrast
agent)가
MRI (26). EPI
(temporal resolution) MRI
(susceptibility effect) 가
EPI EPI EPI
, T2*
Reimer (26)
T2* 가
, T2 , T2*
가 10%
T2* EPI

- 1.5 T. *Radiology* 1990;176:211-220
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Assessment of Neoplastic Angiogenesis Using Perfusion-Weighted MR Imaging: Experimental Study in VX2 Carcinoma in Rabbits¹

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Purpose: To evaluate the perfusion-weighted MR imaging findings of hepatic VX2 carcinoma in rabbits and to explain the perfusion characteristics of this condition by correlation with the histopathological findings.

Materials and Methods: Twelve New Zealand white rabbits, each weighing between 2.5 and 3.5 (mean) 3.1 kg, were used in this study. Perfusion MRI using single-shot gradient-echo EPI was performed 7 - 21 days after the injection of tumor cell suspension into the hepatic parenchyma by laparotomy. On the basis of the calculated enhancement ratio, the time-intensity perfusion curves for VX2 tumor and normal liver parenchyma were created, and the shapes of these curves, the time to maximum SI decrease, and the maximum enhancement ratio in each, were evaluated. To assess microvessel density in each VX2 carcinoma and in normal liver parenchyma, immunohistochemical study using factor VIII-related antigen was performed.

Results: A total of 15 tumors 1 - 3 cm in diameter were revealed by MR imaging. The perfusion curve showed rapid decrement and immediate recovery of the signal intensity of VX2 carcinoma during the early arterial perfusion phase and slower decrement and gradual recovery of that of normal liver parenchyma during the late portal perfusion phase. In all cases, these were constant findings. The time to maximum signal intensity decrease was 13 - 16 (mean, 15) secs in VX2 carcinoma and 28 - 36 (mean, 32) secs in normal liver parenchyma ($p < 0.01$). The maximum enhancement ratio of VX2 carcinoma and normal liver ranged from 27 to 84% (mean 47%) and from 36 to 82% (mean, 56%), respectively. Immunohistochemical study showed that the MVD of VX2 carcinoma was significantly greater than that of normal liver parenchyma (75 vs 17, $p < 0.01$).

Conclusion: Perfusion-weighted MR imaging appears to be a useful tool for the diagnosis of neoplastic angiogenesis, and thus holds promise differentiating liver tumors.

Index words : Magnetic resonance (MR), perfusion study

Liver neoplasms, MR

Neoplasms, MR

Neoplasms, experimental studies

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