

ADC map trace map

single-shot EPI b-factor (DWI)

(X, Y, Z)

ADC map ADC

trace (ROI)

trace map ADC map

(anisotropic diffusion)

3 15

(n=10) (n=5)

trace ADC

trace / (trace) 0.995 ± 0.031 ADC

(ADC) Dxx 가 0.980 ± 0.098 , Dyy 가 1.019 ± 0.086 , Dzz 가 0.999 ± 0.111

trace 가 1.001 ± 0.028 , Dxx 가 1.001 ± 0.058 , Dyy 가 0.996 ± 0.063 , Dzz 가 1.005 ± 0.070

trace 가 1.007 ± 0.021 , Dxx 가 1.002 ± 0.064 , Dyy 가 1.023 ± 0.055 , Dzz 가 0.999 ± 0.060

trace 가 0.05 ADC

trace 가 ADC

ADC 가 ($p < 0.05$)

가 ($p < 0.05$).

: Trace map ADC map trace 가 ADC

ADC map ADC map

ADC map 가 trace map ADC map

180°

(motion artifact)

EPI 가

가 T1, T2, (post-image processing) (apparent diffusion coefficient map, ADC map) 가 (1- 2) ADC map 가 (anisotropic diffusion) 가 (3). ADC map (X, Y, Z) ADC map trace (Trace = Dxx + Dyy + Dzz) trace map ADC map (4-5).

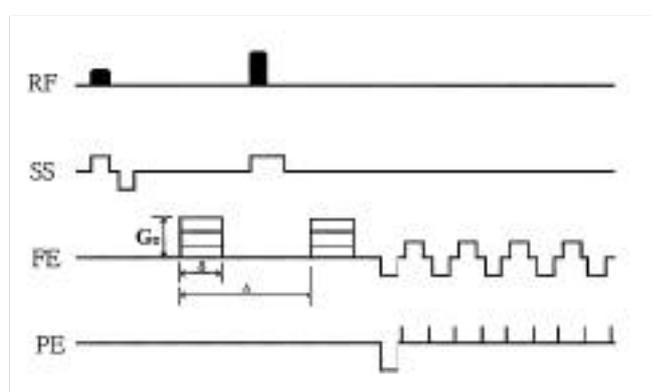


Fig. 1. Diffusion weighted single-shot EPI pulse sequence. (RF - resonance frequency pulse, SS - slice selection pulse, FE - frequency encoding pulse, PE - phase encoding pulse)

ADC Map Trace Map 가 ADC map trace map 가 , 가 가 ADC map trace map 가 1997 5 7 가 18 ADC map trace map 29 85 56.7 가 12 가 6 가 4 가 6 가 6 48 48 10 10 4 12 1 1.5T imager (Horizon, GE Medical System, Milwaukee, Wisconsin, USA) single-shot EPI 180° 31msec EPI FOV 20-24cm, TR 6500ms, TE 120ms, 7mm, 3mm, 128 x 128 matrix, 1 NEX, 14-15 slices b-factor 0, 333, 666, 1000s/mm² 4 (X - frequency encoding, Y - phase encoding, Z - slice selection) 180° 31msec (Fig.1). 10 b-factor가 0s/mm² b-factor 333, 666, 1000s/mm² 9) 14 ~ 15 (Fig. 2). ADC map IDL (Research System Inc., Colorado, USA) Sun (SUN Micro System Inc., California, USA) PC 가 b-factor 가 (S) Stejskal-Tanner (1)(6) (D)

$$S(TE, b) = S_0 e^{-TE/T_2 - bD}$$

$$\ln S(TE, b) = \ln S_0 - TE/T_2 - bD$$

$$D = -\ln\{S(TE, b)/S(TE, 0)\}/b$$

[1]

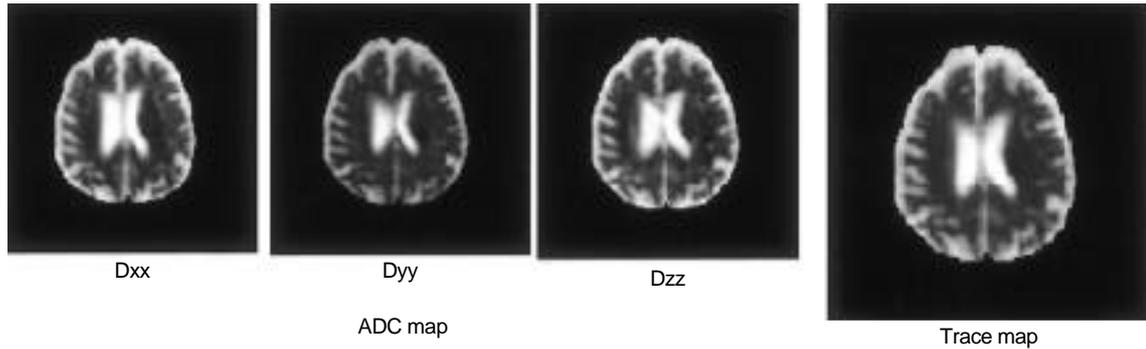


Fig. 3. ADC map and Trace map of the brain of subject 14 who had symptom of dysarthria 107 hours before MRI was taken. ADC maps were obtained by homemade post-image processing program on the basis of Stejskal-Tanner equation[1]. Trace map was obtained by also another homemade post-image processing program using the sum of Dxx, Dyy, and Dzz pixel by pixel. The infarct area shows dark signal intensity on these images in contrast to the DWI. Note that the differentiation of white matter and gray matter, which is demonstrated in the ADC maps, is not visualized in the trace map.

Table 1. Summary of Patients

	Sex	Age	Stage	Interval	Location
S1	F	85	hyperacute	5hr	Both thalamus
S2	M	69	acute	28hr	Lt. DWM
S3	M	52	acute	32hr	Lt. LN
S4	M	67	acute	38hr	Lt. thalamus
S5	F	66	acute	44hr	Lt. GM & DWM
S6	M	60	subacute	2.4d	Both PVWM
S7	M	29	subacute	2.8d	Lt. GM & DWM
S8	F	63	subacute	2.8d	Lt. LN
S9	M	50	subacute	2.8d	Rt. PVWM
S10	M	43	subacute	3.0d	Lt. posterior internal capsule
S11	M	40	subacute	3.4d	Rt. LN
S12	M	34	subacute	3.8d	Rt. PVWM
S13	M	52	subacute	4.3d	Rt. PVWM
S14	M	60	subacute	4.5d	Lt. PVWM
S15	M	57	subacute	5.0d	Lt. PVWM
S16	F	67	subacute	5.8d	Rt. GM & DWM
S17	F	76	subacute	7.7d	Rt. DWM
S18	F	51	chronic	394.3d	Lt. PVWM

Interval - time interval between the onset of symptoms and the time of taking diffusion images, Location - the site of infarct lesion GM - gray matter, WM - white matter, DWM - deep white matter, PVWM - periventricular white matter, LN - lentiform nucleus

가 , 가 ,
 가 .
 , 가 t-test .
 . 18 [4]
 ADC trace 가
 (average . (n=10)
 deviation, AD) (n=5) , 3 (Table 1 - S5, S7,
 (AD_{WM}, AD_{GM}, AD_{CSF}) S16)
 (Table 2,3,4). 가

$$AD = (|Dxx \text{ ratio} - \text{Trace ratio}| + |Dyy \text{ ratio} - \text{Trace ratio}| + |Dzz \text{ ratio} - \text{Trace ratio}|) / 3 \quad [4]$$

Mackintosh PC NIH

ADC trace
 (Fig. 4).

Table 4. Rt/Lt Dxx, Dyy, Dzz, Trace Ratios and Average Deviation of Normal CSF

	Dxx ratio	Dyy ratio	Dzz ratio	Trace ratio	AD _{CSF}
S1	1.133	0.959	0.941	1.020	0.084
S2	1.148	1.030	0.966	1.042	0.065
S3	0.929	1.031	0.996	0.988	0.037
S4	0.968	1.027	0.995	0.998	0.021
S5	0.932	0.982	0.995	0.969	0.025
S6	0.943	1.019	1.027	0.997	0.035
S7	0.998	1.022	0.984	1.000	0.013
S8	0.984	1.022	1.023	1.004	0.019
S9	0.981	1.111	1.067	1.028	0.056
S10	1.016	0.915	1.104	1.008	0.066
S11	0.976	1.056	1.054	1.025	0.036
S12	0.942	1.057	1.010	1.001	0.041
S13	1.101	0.995	1.006	1.031	0.044
S14	1.000	0.967	0.945	0.970	0.019
S15	1.019	1.080	0.891	0.996	0.071
S16	0.990	1.116	0.878	0.998	0.082
S17	0.983	0.945	1.034	1.003	0.036
S18	0.985	1.073	1.069	1.043	0.038
Average	1.002	1.023	0.999	1.007	0.044
SD	0.064	0.055	0.060	0.021	0.022

AD_{CSF} - average deviation of normal CSF,
SD - standard deviation

periventricular white matter(n=7), deep white matter(n=2) internal capsule(n=1) (Table 1).

ADC trace ADC trace
0.980 1.023
ADC trace ADC
Dxx, Dyy, Dzz 0.098,
0.086, 0.111 (Table 2, Fig. 5), 0.058, 0.063, 0.070
(Table 3, Fig. 6), 0.064, 0.055, 0.060
(Table4, Fig. 7) 0.05 trace
0.031, 0.028, 0.021

0.05 가 . ,
trace 10% trace 가 ADC
ADC 10% 가

가 가
trace 3 ADC

가
0.072 ± 0.034 (Table 2),
0.043 ± 0.020 (Table 3), 0.044 ± 0.022
(Table 4). paired t-test

p-value가 0.05 (: p = 0.009, : p = 0.013)

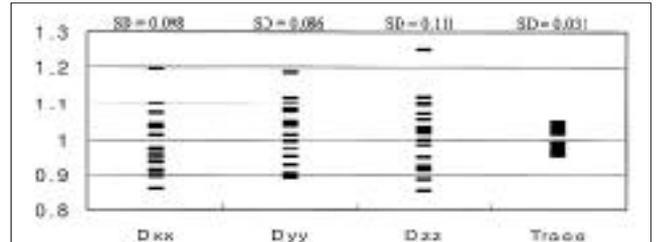


Fig. 5. Dxx, Dyy, Dzz and Trace ratios of White matter

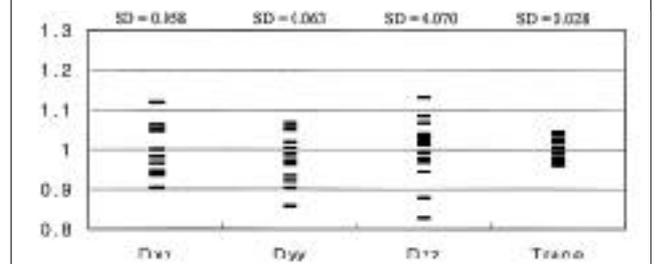


Fig. 6. Dxx, Dyy, Dzz and Trace ratios of Gray matter

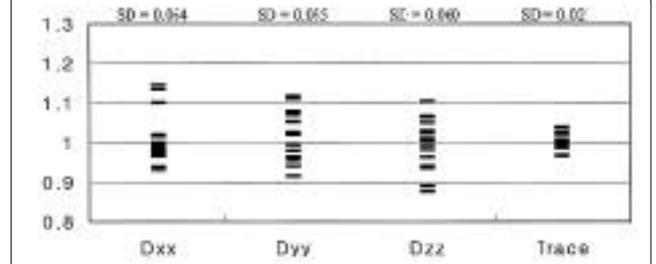


Fig. 7. Dxx, Dyy, Dzz and Trace ratios of CSF

Fig. 5, 6, 7. All trace ratios are concentrated on the range of 10% around the average(1 ± 0.05). But, ADC ratios are more scattered significantly than trace ratios. Therefore, trace ratio is more accurate representative value than ADC ratio(SD - standard deviation).

가 , 가 (p=0.943).

가

ADC trace 가 가

0.116 ± 0.053 (Table 5)

가 0.045 ± 0.017 (Table 6)

ADC 가 t-test
p-value가 0.012

가 ADC 가

Table 5. Ipsilateral/Contralateral Dxx, Dyy, Dzz, Trace Ratios and Average Deviation of White Matter Involved Infarct

	Dxx ratio	Dyy ratio	Dzz ratio	Trace ratio	AD _{WM-inf}
S2	0.542	0.577	0.648	0.591	0.040
S6	0.628	0.604	0.839	0.692	0.100
S9	0.932	0.828	0.508	0.747	0.168
S10	0.81	0.624	0.418	0.621	0.132
S12	0.995	1.223	1.094	1.086	0.079
S13	0.627	0.72	0.886	0.723	0.087
S14	0.601	0.821	0.735	0.702	0.084
S15	0.528	0.568	0.742	0.619	0.088
S17	0.55	0.943	0.88	0.755	0.173
S18	1.825	2.297	1.791	1.952	0.211
Average					0.116
SD					0.053

AD_{WM-inf} - average deviation of white matter infarct,
SD - standard deviation

Table 6. Ipsilateral/Contralateral Dxx, Dyy, Dzz, Trace Ratios and Average Deviation of Gray Matter Involved Infarct

	Dxx ratio	Dyy ratio	Dzz ratio	Trace ratio	AD _{GM-inf}
S1	0.704	0.661	0.701	0.689	0.018
S3	0.623	0.642	0.723	0.664	0.041
S4	0.601	0.544	0.43	0.522	0.064
S8	0.735	0.806	0.667	0.719	0.052
S11	0.959	0.907	1.048	0.963	0.048
Average					0.045
SD					0.017

AD_{GM-inf} - average deviation of gray matter infarct,
SD - standard deviation

가
cytotoxic edem (7),
T1, T2,

, ADC map

12 -24 가
가 1-2
(Pseudo-normalization),
가

가 ADC map
(1).

가
(brain perfusion scan)

(ischemic penumbra)
ADC map 가
, ADC
가
가 (8)
ADC
absolute diffusion constant ($D_{av} = Tr/3$)
trace
diffusion time(t_{diff})
 t_{diff} 가 D_{av} 가
(5, 8, 9).
Ulug absolute diffusion constant
(hemispheric ratio for $D_{av} = (1/C)D_{av}$)
(10). absolute diffusion constant
(Ipsilateral)/ (Contralateral) (1/C ratio)
diffusion time absolute diffusion constant
가
ADC map trace map
Ulug
trace /
Ulug가 6
6
trace map trace ADC map
olute diffusion constant 가 ab-
가 0.05
ADC map Dxx, Dyy, Dzz
(10)
가
0.771 ± 0.094s/mm² 0.742 ± 0.054s/mm²,
3.177 ± 0.465s/mm²
가 (p > 0.05),
가

($p < 0.01$).

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Comparison of ADC Map with Trace Map in the Normal and Infarct Areas of the Brains of Stroke Patients¹

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Purpose : To compare ADC mapping with trace mapping in normal and infarct areas of the brains of stroke patients.

Materials and Methods : Eighteen patients diagnosed on the basis of clinical and brain MRI examinations as suffering from brain infarction were included in this study (hyperacute-1, acute-4, subacute-12, chronic-1). Diffusion weighted images of three orthogonal directions of a patient's brain were obtained by means of a single shot EPI pulse sequence, using a diffusion gradient with four serial b-factors. Three ADC maps were then reconstructed by post-image processing and were summed pixel by pixel to yield a trace map.

ROIs were selected in the normal areas of white matter, gray matter and CSF of one hemisphere, and other ROIs of the same size were selected at the same site of the contralateral hemisphere. ADC and trace values were measured and right/left ratios of ADC and trace values were calculated. Using these values, we then compared the ADC map with the trace map, and compared the degree of anisotropic diffusion between white matter, gray matter and CSF.

Except for three, whose infarct lesions were small and lay over white and gray matter, patients were divided into two groups. Those with infarct in the white matter (n= 10) were assigned to one group, and those with infarct in the gray matter (n= 5) to the other. ROIs were selected in the infarct area and other ROIs of the same size were selected at the same site of the contralateral hemisphere. ADC and trace values were measured and infarct/contralateral ratios were calculated. We then compared ADC ratio with trace ratio in white matter and gray matter infarct.

Results : In normal white matter, the Dxx ratio was 0.980 ± 0.098 , the Dyy ratio 1.019 ± 0.086 , the Dzz ratio 0.999 ± 0.111 , and the trace ratio 0.995 ± 0.031 . In normal gray matter, the Dxx ratio was 1.001 ± 0.058 , the Dyy ratio 0.996 ± 0.063 , Dzz ratio 1.005 ± 0.070 , and the trace ratio 1.001 ± 0.028 . In CSF, the Dxx ratio was 1.002 ± 0.064 , the Dyy ratio 1.023 ± 0.055 , the Dzz ratio 0.999 ± 0.060 and the trace ratio 1.007 ± 0.021 . Because the standard deviation of trace ratios (< 0.05) is less than that of ADC ratios (> 0.05), the trace ratio is more accurate representative value.

The standard deviation of white matter is greater than that of gray matter or CSF ($p < 0.05$), the degree of anisotropic diffusion in white matter is therefore more severe than in gray matter and CSF.

The difference between the ADC ratios and trace ratio is greater in an infarct involving white matter than in one involving gray matter ($p < 0.05$).

Conclusion : Because a trace map overcomes the anisotropic diffusions of ADC maps, the former offers better post-image processing.

The deviation of ADC ratios owing to the direction of diffusion gradient is greater in white matter than in gray matter, and the trace map is thus superior for evaluation of an infarct involving white matter.

Index words : Brain, MR

Brain, stroke

Magnetic resonance(MR), diffusion study

Magnetic resonance(MR), technology