

Recent Advances for Enhancing Drug Metabolizing Functions of Hepatocyte-like Cells Derived from Human Pluripotent Stem Cells

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Hepatocyte-like cells (HLCs) derived from human pluripotent stem cells are a promising cell source for drug screening and toxicity tests. Thus, various hepatic differentiating protocols have been developed, leading to a hepatic differentiation efficiency of approximately 90%. However, HLC drug metabolizing ability remains very low compared to human primary hepatocytes. In order to overcome this problem, several alternative methods, such as, co-culture, three-dimensional (3D) culture, bioreactor, nanochip-based, etc., have been developed, but optimization to produce fully functional HLCs is ongoing. Recently, our group reported that repeated exposure of HLCs to xenobiotics can improve the expression of hepatic metabolizing enzymes such as cytochrome P450s (CYPs) and glutathione S-transferases (GSTs). These data suggest that we should develop strategies for differentiating cells into mature HLCs by more closely mimicking *in vivo* fetal and postnatal liver development. Here, we review the current development of alternative methods for enhancing the drug metabolizing functions of HLCs derived from human embryonic stem cells, human-induced pluripotent stem cells, and mesenchymal stem cells as used for drug screening and toxicity tests.

Key Words: Bioreactors; Coculture Techniques; Hepatocytes; Stem Cells

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INTRODUCTION

Clinical treatment for chronic liver failure using human embryonic stem cell (hESC) and human-induced pluripotent stem cell (hiPSC)-derived hepatocyte-like cells (HLCs) is considered a promising alternative method to organ transplantation. In addition to their use for treatment in liver failure, stem cell-derived HLCs have been considered for *in vitro* drug screening and toxicology researches [1]. Therefore, HLCs directly induced from hESCs have been intensively studied, resulting in a significant improvement in the efficiency of hepatic differentiation using human pluripotent stem cells. Albumin-positive HLCs can now be produced at the end of *in vitro* hepatic differentiation at levels up to 90% [2,3]. How-

ever, in spite of efforts to induce further maturation of HLCs derived from human pluripotent stem cells, the phenotype of most HLCs is more similar to fetal hepatocytes rather than fully mature hepatocytes. Critical inducing mature hepatocyte functions, such as phase I and II enzyme activity, tend to be significantly reduced in 2D-cultured HLCs (approximately < 1% of human primary hepatocytes) [4,5]. Furthermore, under *in vitro* culture conditions, hepatobiliary transporter expression rapidly decreases [6], and most HLCs are spontaneously differentiate into various cell lineages, regardless of the differentiation protocol. Thus, at the final stage of hepatic differentiation, purification is needed to obtain highly homogenous HLCs. These key differences between HLCs and human primary hepatocytes result in limited use of HLCs as

a renewable cell source of functional adult hepatocytes for cell transplantation and *in vitro* toxicity tests. The low metabolizing ability and limited *in vitro* culture duration of HLCs must be overcome prior to using HLCs for clinical applications and *in vitro* drug screening and toxicology researches.

A lack of knowledge regarding the developmental signaling pathways that control *in vivo* hepatic maturation contributes to the development of immature HLCs, which usually display a fetal phenotype. Therefore, in this review paper, we will discuss current hepatic differentiation culture systems that enhance hepatic maturation of HLCs and gain a metabolizing response against xenobiotics at a level similar to that of human primary hepatocytes.

ALTERNATIVE CULTURE SYSTEMS TO ENHANCE HEPATIC FUNCTIONS

1. Co-culture system

During organogenesis, differentiation of pluripotent cells into functional hepatocytes is controlled by a complex signaling pathway of molecular events. Therefore, the most direct way of inducing hepatic differentiation is to mimic the *in vivo* signaling pathway present during liver development. Studies have clearly defined many of these molecular events, such as reduced Oct4 activity, which allows for the activation of FoxA2 (HNF3 β), SOX17, and GATA4, a process necessary for the differentiation of endodermal cells into hepatocytes [7]. Fair et al. reported that murine ESCs in co-culture with chick cardiac mesodermal cells were successfully differentiated into early hepatocyte lineage as determined by morphology and induction of HNF3 β , SOX17, and GATA4 genes [7]. Furthermore, cardiac mesodermal cells can be stimulated to form hepatic progenitor colonies *in vitro*. Cardiac mesoderm cells are used for hepatic differentiation because their fibroblast growth factor (FGF 1 and 2) induces competent foregut endodermal cells, which are further differentiated into hepatocytes [7]. As our knowledge of liver development during organogenesis increases, more developmentally correlated co-culture systems can be established for hepatic maturation of HLCs.

Liver parenchyma consists of 80% hepatocytes (polyploidy epithelial cells) in addition to several different types of cells such as endothelial cells, Kupffer cells, and stellate cells [8]. Together, these cells harmonize to maintain homeostatic liver functions including a response against xenobiotics, both initially as well as to repeated exposure. For example, endothelial cells often called “sinusoids”

distribute blood throughout the liver. Hepatic macrophages, or Kupffer cells, ingest foreign molecules (xenobiotics and nutrients) and charge for an immune response. Additionally, stellate cells, or Ito cells, serve to store fat in the liver when they are in a resting state, where they produce rich extracellular matrix (ECM) for tissue regeneration.

The liver possesses an amazing capacity for regeneration. As a result of liver damage or hepatectomy due to liver cancer *in vivo*, a liver can regenerate up to approximately 75% of its original volume and double its size within four weeks. Major cytokines produced by surrounding cells of hepatocytes are tumor necrosis factor alpha (TNF α) and interleukin (IL)-1, IL-6, IL-8, IL-10 by Kupffer cells, and transforming growth factor beta (TGF β) by activated stellate cells [9]. Many researchers speculate that this kind of regeneration is accomplished by cell-cell interactions and cytokines and growth factors produced from various surrounding cells. Based on this idea, numerous studies have examined hepatic functions of HLCs co-cultured with mesenchymal stem cells of various origins and stromal cells such as fibroblasts and endothelial cells [10]. A recent study reported that a combination of cell-cell interaction using micro-patterned dishes and co-culture with murine embryonic fibroblasts significantly increased gene expression and activity of hepatic drug metabolizing enzymes (Phase I and II) in HLCs as well as long-term culture (a month) [11].

Disadvantages of a co-culture system are the presence of difficult-to-define inducing factors as well as the need for another cell source for hepatic maturation of HLCs. Additionally, at the final stage of hepatic differentiation, a purification procedure is required to discard co-cultured cells and to harvest homogenous HLCs.

2. 3D culture system

Organogenesis takes place in a 3D manner, with cell-cell interaction occurring on an ECM structure rather than a 2D flat sheet [12]. However, since Reid et al. characterized monolayer-cultured human primary hepatocytes *in vitro*, numerous studies have investigated ways to improve hepatic functions of not only human primary hepatocytes but also HLCs *in vitro* [13]. There have been several recent molecular mechanistic studies and genetic and protein profiling analysis using the 3D culture model to further understand hepatic development and enhance maturation of hepatic enzyme functionality. Generally, 3D-cultured hepatocytes have long-term expression of albumin-positive HLCs with increased hepatic metabolizing enzymes and multidrug resistance proteins

Table 1. Recently reported CYP450 expression and activity in human pluripotent stem cell-derived hepatocyte-like cells

| No. | Year | Cell sources | 2D vs 3D | CYP enzymes | Expression | | | Activity Inducer | References |
|-----|------|---|----------|---|------------|-----------|---|--|------------|
| | | | | | PCR | Western | Array | | |
| 1 | 2015 | hiESC | 2D | CYP1A1, CYP1A2, CYP1B1, CYP2E1, CYP2B6, CYP2D6, CYP2C9, CYP2C19, CYP3A4, CYP7A1 | ✓ | | | [14] | |
| 2 | 2015 | hiESC, hiPSC | 2D vs 3D | CYP1A2, CYP3A4, CYP3A7, CYP2D6, CYP2C9, CYP2C19 | ✓ | IHC | P450-Glo assay | Rifampicin, phenobarbital, acetaminophen | [2] |
| 3 | 2015 | hiESC | 2D | CYP7A1, CYP3A4 | ✓ | | | | [15] |
| 4 | 2014 | hiESC | 2D | CYP1A1, CYP1A2, CYP2B6, CYP3A4 | ✓ | IHC | | | [16] |
| 5 | 2014 | hiESC | 2D | CYP3A4, CYP3A7 | ✓ | | | | [17] |
| 6 | 2014 | Placenta derived human amniotic epithelial cells (hAEC) | 3D | CYP3A4 | ✓ | | P450-Glo assay | | [18] |
| 7 | 2014 | hiESC | 3D | CYP1A1, CYP1A2-β, CYP2B6, CYP2B7 | | | Penthoxyresorufin-O-deethylase (PROD), ethoxyresorufin-O-deethylase (EROD) assay | CYP1A1, CYP1A2-β induced by naphthoflavone 50 μM, CYP2B6, CYP2B7 not changed by phenobarbital 500 μM | [19] |
| 8 | 2014 | hiESC | 3D | CYP3A4 | ✓ | IHC | P450-Glo assay | | [20] |
| 9 | 2014 | hAdipose-derived Stem cells | 2D | CYP1A1, CYP1A2, CYP2B1/2 | ✓ | | Methoxyresorufin-O-deethylase (MROD), PROD, EROD | | [21] |
| 10 | 2014 | hiPSC | 3D | CYP3A4 | ✓ | | P450-Glo assay | | [22] |
| 11 | 2013 | hiPSC | 2D | CYP3A4 | | | | Omeprazole (50 μM), rifampicin(40 μM), dexamethasone (100 μM) | [23] |
| 12 | 2013 | hiESC, hiPSC | 2D | CYP1A, CYP2B6, CYP2C9, CYP3A | ✓ | | LC/MS analysis | Phenacetin (220 μL), bupropion (100 μM), diclofenac (9 μM), midazolam (3 μM) | [24] |
| 13 | 2013 | hiPSC | 2D | CYP3A4, CYP3A7, CYP7A1 | ✓ | | | After removed oncostatin M from medium, then increased gene expression | [25] |
| 14 | 2013 | hiPSC | 2D | CYP1A1, CYP2C9, CYP2C19, CYP3A4, CYP7A1 | ✓ | | P450-Glo CYP3A4 assay | Rifampicin (25 μM), phenobarbital (500 μM) | [26] |
| 15 | 2013 | Human umbilical cord-derived mesenchymal stem cells | 2D | CYP1A2, CYP2C9, CYP2D6, CYP3A4 | ✓ | | LC/MS analysis | Testosterone | [27] |
| 16 | 2013 | Menstrual blood-derived mesenchymal stem cells | 2D | CYP1A1, CYP3A4 | ✓ | IHC | | | [28] |
| 17 | 2013 | Human bone marrow mesenchymal stem cells | 2D | CYP2B | | | | Phenobarbital (2 mM) | [29] |
| 18 | 2013 | hiPSC | 2D | CYP1A1 | | | EROD for CYP1A1 | Ethoxyresorufin (8 μM), dicumarol (10 μM) | [30] |
| 19 | 2013 | Lentivectors encoding green fluorescent protein (GFP) driven by the liver-specific apolipoprotein A-II (APOA-II) promoter to purify human hepatic progenitors | 2D | CYP3A4 | | FAUS, IHC | Expression of green fluorescent protein (GFP) driven by the cytochrome P450 3A4 (CYP3A4) promoter in purified hepatocyte-like cells | | [31] |

(Continued to the next page)

Table 1. Continued

| No. | Year | Cell sources | 2D vs 3D | CYP enzymes | Expression | | | Activity Inducer | References |
|-----|------|---|----------|---|------------|--|-----------------------|------------------|------------|
| | | | | | PCR | Western | Array | | |
| 20 | 2013 | hiPSC | 2D | CYP1A1, CYP1A2, CYP2C9, CYP2C19, CYP2D6, CYP3A4, CYP3A7, CYP7A1 | ✓ | Comparison of gene expression to HepG2 | | [32] | |
| 21 | 2013 | Primary human hepatocyte | 2D vs 3D | CYP2E1 | ✓ | | Acetaminophen | [33] | |
| 22 | 2013 | primary parenchymal and non-parenchymal hepatic cells | 2D vs 3D | | ✓ | | | [34] | |
| 23 | 2013 | hiESC | 2D vs 3D | CYP3A4, CYP7A1 | ✓ | | | [35] | |
| 24 | 2013 | Human pluripotent stem cells | 3D | | | PROD test | Rifampicin (25 µM) | [36] | |
| 25 | 2012 | hiPSC | 2D | CYP3A4, CYP7A1 | ✓ | | | [37] | |
| 26 | 2012 | hiPSC | 2D | CYP3A4, CYP2C19 | ✓ | | | [38] | |
| 27 | 2012 | Human Fetal Hepatic Progenitor Cell (hFHPCs) | 2D | CYP1A1, CYP1A2, CYP2B1/2 | ✓ | | Pentoxifylline (1 µM) | [39] | |

hiESC, human embryonic stem cells; iPSC, induced pluripotent stem cells.

(MRPs). 3D-cultured HLCs have noticeable advances in hepatic differentiation and maturation, which retain many *in vivo*-like properties [6].

Typical 2D culture may disrupt the complex microenvironment of an *in vivo* liver, resulting in the loss of liver architecture. Thus, even though the efficiency of hepatic differentiation is high in most directly induced HLCs, few studies have reported fully functional HLCs. Instead, many studies have utilized the 3D spheroid formation of hESCs, hepatoblast, or immature HLCs for hepatic maturation. Table 1 summarizes recent studies that report on either gene expression or activity of hepatic metabolizing enzymes of human pluripotent stem cell-derived HLCs using a 2D or 3D culture system. Interestingly, a few studies measure both protein levels of metabolizing enzymes and activity of induced enzymes. Various 3D culture systems have been developed for hepatic differentiation such as ultra-low attached dish, microsound bottom well plate, porous scaffold, nanopattern chip, droplet culture, and ECM.

Our group reported on HLC culturing using 3D embryonic body (EB) and 3D cultured definitive endodermal spheroid formation with lithium chloride [40,41]. However, it was difficult to prevent spontaneous differentiation during EB- or 3D cultured hepatic spheroid-mediated induction. Therefore, a purification procedure at the final stage of hepatic differentiation was needed to obtain homogenous HLCs. Most importantly, the expression of a typical hepatic cytochrome P450 (CYP)3A4 was still low, and its activity was increased -1.5 times by acetaminophen treatment. Recently, we successfully optimized our protocol and our >90% of albumin-positive HLCs were produced (Fig. 1). However, expression and activity of hepatic metabolizing enzymes in 2D cultured HLCs were much more improved but still not reached the levels of human primary hepatocytes. Therefore, we further enhanced the hepatic metabolizing ability of HLCs using a 3D culture system and repeated exposure to xenobiotics (Fig. 2,3)[8].

A disadvantage of using a 3D culture system is that HLCs, which are at the core of 3D cell clumps or spheroids, can easily undergo apoptosis due to hypoxic conditions and lack of nutrient penetration. Apoptosis of HLCs in a 3D spheroid of approximately >300 µm in diameter begins to increase. Therefore, it is important to optimize the homogenous size of 3D hepatic spheroids.

3. Bioreactor

Bioreactor refers to a manufactured or engineered device pro-

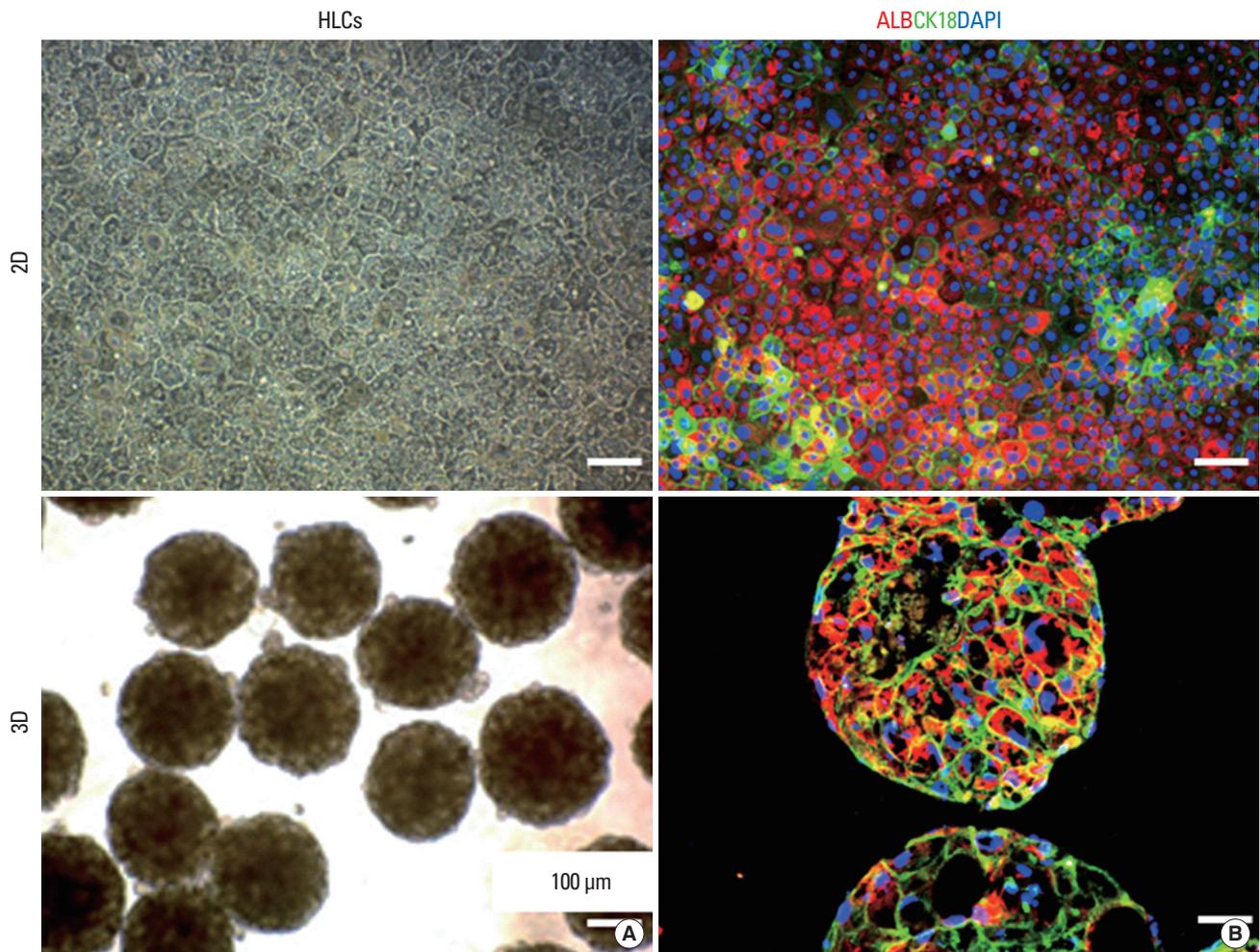


Fig. 1. (A) Characterization of 2D and 3D cultured HLCs. Phase contrast images of HLCs and (B) immunofluorescent images of hepatic markers (ALB: red and CK18: green) in HLCs at the final stage III of hepatic differentiation. Note that 3D hepatic spheroids were formed and further differentiated from single-cell dissociated 2D hepablast. HLCs, hepatocyte-like cells; 3D, three-dimensional.

ducing HLCs under conditions mimicking a biologically active environment in an *in vitro* cell culture system. There are several different types of bioreactors such as, stirred-tank, airlift, waved, hollow-fiber etc. Key points of successful parameters for optimized bioreactors to produce massive scale HLCs are 1) detection of homogenous cell growth, 2) rate of oxygen transfer, and 3) density of maximum final cells [42]. Among the several different types of bioreactors, a simple rotating perfused bioreactor can be used with decentralized growth factors and cytokines as well as a sustained gas supply. One of the significant differences between a 3D culture system and a bioreactor is that bioreactor provides a fluidic, dynamic environment for HLCs, whereas the 3D culture system does not. The reported optimal speed of a rotating bioreactor for 3D cultured hepatic spheroids or HLCs is generally 15-20 rpm [43]. A study reported that human primary hepatocytes cultured

in microgravity-simulated bioreactors formed multi-dimensional tissue-like spheroids [44]. The size of spheroids was up to 1.0 cm and the cells were arranged with biliary epithelial cells as similar as bile duct-like structures and vascular sprouts. In addition, significantly increased hepatic drug metabolizing CYPs (CYP3A5, CYP2C19, CYP2C18, CYP2C9, and CYP2D6) and MRPs were observed in HLCs cultured by a perfused 3D bioreactor, compared to 2D-cultured HLCs [12].

COMMERCIALY AVAILABLE FUNCTIONAL HLCs

There are several commercially available HLCs derived from human pluripotent stem cells. Table 2 summarizes the major providers, cell types, characteristics, and servicing assays of these available HLCs [4,45-49]. An important factor for producing commer-

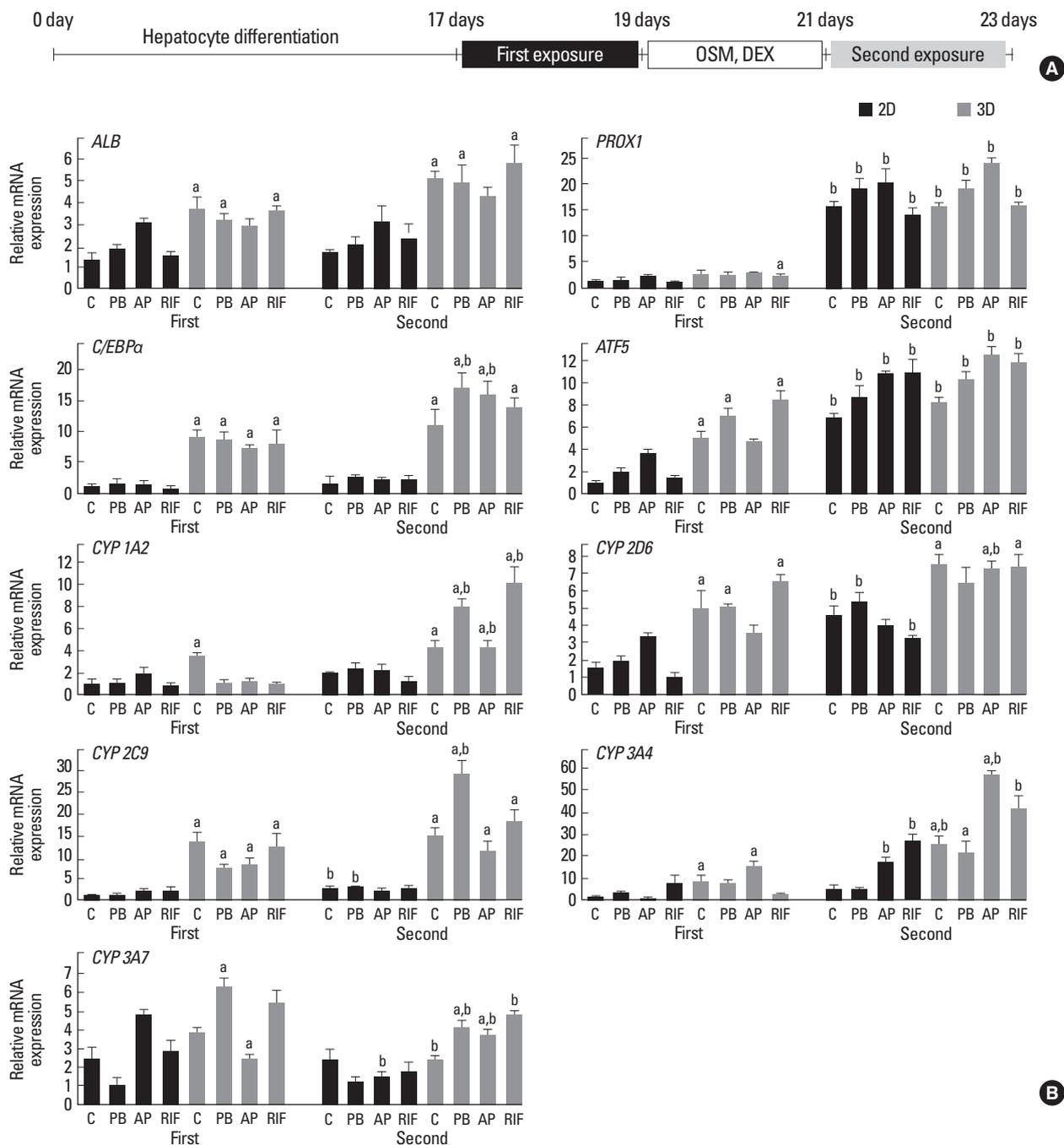


Fig. 2. Enhanced hepatic metabolizing HLCs using 3D culture systems and repeated exposure to xenobiotics. (A) Schematic representation of repeated exposure of 2D-cultured HLCs and 3D hepatic spheroids to xenobiotics. Note that the HLCs and hepatic spheroids derived from BGO1 hESCs were exposed to each xenobiotic concentration at the end of stage III. The xenobiotic treatment was then withdrawn for 2 days followed by a second exposure for 2 days. (B) qPCR analysis of ALB and phase I enzymes (CYP1A2, CYP2D6, CYP2C9, CYP3A4, and CYP3A7) in 2D-cultured HLCs after repeated exposure to xenobiotics. The 'a' denotes statistical significance. Control (C, untreated HLCs); the 'b' denotes statistical significance, compared to the first exposure of its own group. Phenobarbital (PB, widely prescribed as an anti-seizure medication in children); Acetaminophen (AP, a common cold medication); rifampicin (RIF, an antibiotic used to treat infections). OSM, oncostatin M and DEX, dexamethasone. Ref. 2 with permission from Oxford University Press.

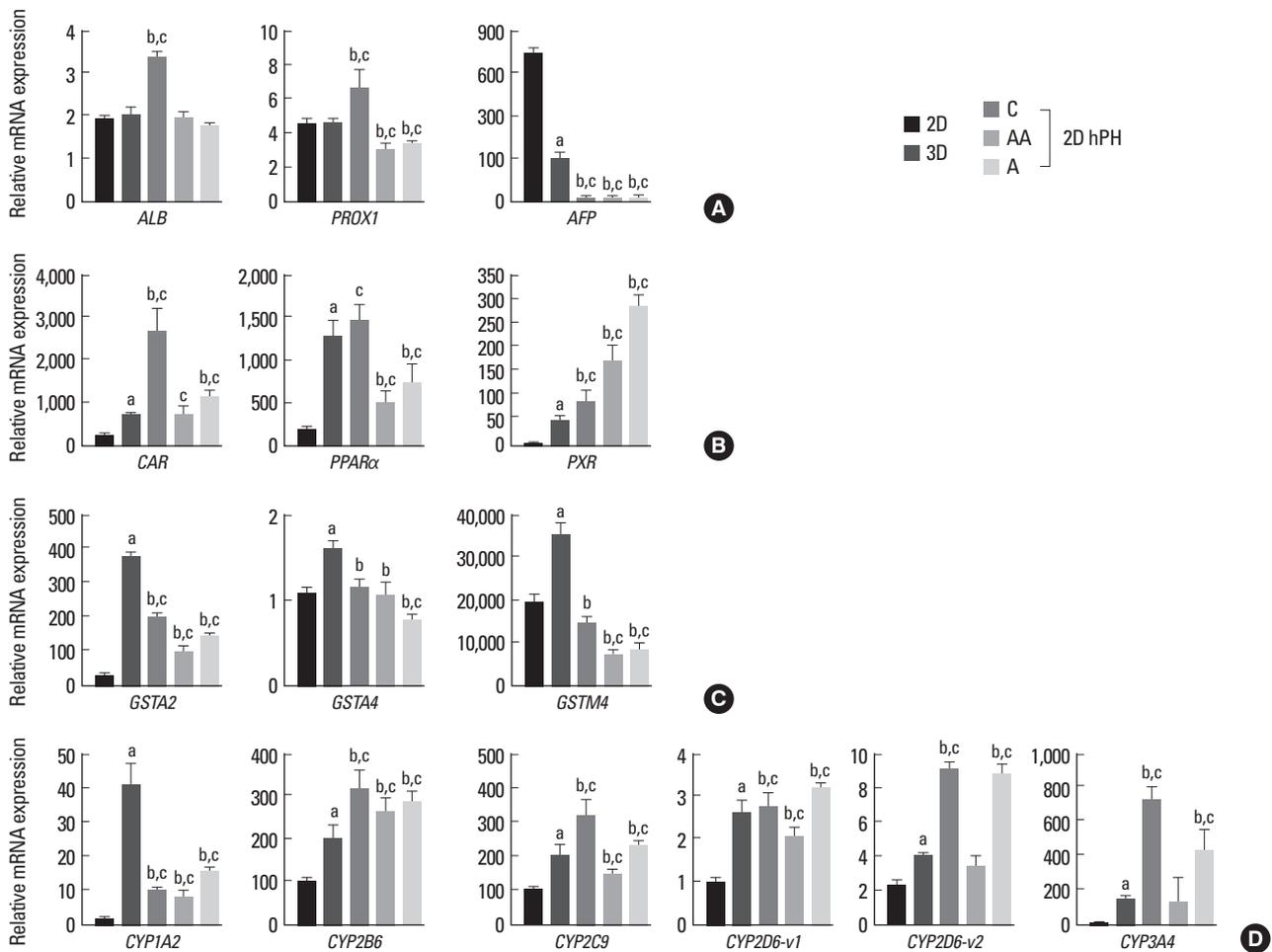


Fig. 3. Comparison of hepatic gene expression among 2D-cultured HLCs (2D), 3D-cultured hepatic spheroids at day 6 of stage III (3D), and three different human primary hepatocytes 24 hours after *in vitro* culture (2D) using qPCR analysis. Each of the 2D-cultured human primary hepatocytes (green bars) were obtained from Caucasian (C), African American (AA), and Asian (A) subjects. Statistical significance is reported as 'a' for statistical significance of gene expression between 2D HLCs and 3D hepatic spheroids, 'b' for statistical significance of gene expression between 3D hepatic spheroids and 2D human primary hepatocytes, and 'c' for statistical significance of gene expression between 2D HLCs and 2D human primary hepatocytes. (A) Expression of ALB (albumin), PROX1, and AFP. (B) Expression of nuclear receptor (NR), which regulate the expression of key hepatic CYP genes. (C) Gene expression of various isoform GSTs, which are part of the GST phase II metabolic enzyme family. (D) Gene expression of hepatic CYPs. Data are presented as the means \pm 6SD of 4 separate experiments. Ref. 2 with permission from Oxford University Press.

cially available HLCs is what will be used for quality control, as they will be used for assays such as drug screening and toxicity tests. For example, proven typical hepatic metabolizing enzyme activities such as of CYP1A2 and CYP3A4 could be used as quality control standards for commercially available HLCs. The cost of a 24- or 96-well plate is approximately \$2,500 if a Korean researcher orders commercially available HLCs from a US provider, and it may take three to six months to receive living HLCs on a plate. None of the major companies provide gene expression profiling of metabolizing enzymes or MRPs of their HLCs. Cellular Dynamics International (CDI), which was founded by James Thomson, reported that their iCell[®] hepatocytes express 1,936 absorption,

distribution, metabolism, and excretion (ADME) markers in over 200 genes, which include all Food and Drug Administration (FDA)-validated genes, but the expressed genes are not reported [45]. Consequently, at this point, it is impractical to use only HLCs to predict and screen the toxicity of new drugs without using human primary hepatocytes as a control. From the point of view of pharmaceutical companies and regulatory agencies, there is no benefit to using high-priced HLCs instead of human primary hepatocytes.

Currently, European and US companies (Cellartis-European, CDI-USA, and Geron-USA) have discontinued production of HLCs. Takara Bio Europe AB acquired Cellectis-European in 2014 and Fujifilm Holdings Corp acquired CDI-USA, thus Japanese com-

Table 2. Commercially developed hepatocytes derived from human pluripotent stem cells

| Company | Country | Pros | Cons |
|---------------------------------|---------|---|--|
| Vistagen Therapeutics | USA | <ul style="list-style-type: none"> LiverSafe 3D™-VSTA-heps™ (HLCs derived from hESCs) for a bioassay system of hepatotoxicity and drug screening Holds several patents for toxicity tests of somatic cells differentiated from hESCs and hiPSCs | <ul style="list-style-type: none"> Does not provide information on CYP and phase II enzyme expression, except for CYP3A4-positive HLCs |
| Cellular Dynamics International | USA | <ul style="list-style-type: none"> >95% pure iCell® hepatocytes produced for drug screening and toxicity tests iCell® Hepatocytes are platable and maintain hepatocyte functions in culture for 1-3 weeks iCell® hepatocytes have been genotyped for 1,936 ADME markers in over 200 genes, including all FDA-validated genes and >90% of the ADME Core markers as defined by the PharmaADME group | <ul style="list-style-type: none"> Does not provide information on CYP, phase II enzymes, or multidrug transporter gene expression or activity Fujifilm Holdings Corp acquired CDI in 2015 |
| HemoGenix | USA | <ul style="list-style-type: none"> A Bioluminomics™ assay platform of hepatocytes derived from hiPSCs provide drug screening and toxicity tests | <ul style="list-style-type: none"> Does not provide information on CYP, phase II enzymes, or multidrug transporter gene expression or activity |
| Geron | USA | <ul style="list-style-type: none"> Development of a platform using hESCs for regenerating cell-based therapeutic agents and drug screening Development of hESC-derived somatic cells for drug screening and toxicity tests with GE Healthcare Holds patents for hESC-derived HLCs as drug screening tools | <ul style="list-style-type: none"> Aborted clinical trials of hESC-derived somatic cells as cell-based therapeutic agents No longer provides HLC-derived human pluripotent stem cells (since 2014) |
| Cellartis by Takara Bio | Japan | <ul style="list-style-type: none"> Highly homogenous (80%) HLCs derived from hESCs and hiPSCs are produced Cellartis® Enhanced hiPS-HEP (human iPS-derived cells) and hES-HEPTM for drug screening and toxicity tests Cellartis® Enhanced hiPS-HEP: Stable CYP1A, CYP2B6, CYP2C9, CYP2C19, CYP2D6, CYP2E1, and CYP3A activity for up to 8 days (post-recovery) suitable for metabolic toxicity and chronic toxicity tests hES-HEPTM: CYP1A and CYP3A Fresh and frozen cells provided Drug-induced steatosis assay | <ul style="list-style-type: none"> Cellartis (Sweden, England, and France) no longer provides HLC-derived human pluripotent stem cells (since 2014) Takara Bio acquired stem cell unit from Cellartis (Sweden) in 2014 |
| ReproCELL | Japan | <ul style="list-style-type: none"> ReproHepato™: The world's first commercial hiPSC-hepatocytes provide for drug screening and toxicity tests ReproHepato™ has robust enzymatic activity (99.3% of CYP3A4-positive cells) ReproHepato™ also expresses CYP1A2, CYP2C9, CYP2C19, and CYP2D6 | <ul style="list-style-type: none"> CYP and hepatotoxicity assay services are provided only in Japan After six days in culture using maintenance medium provided by ReproCELL, the HLCs are ready to use |

panies (ReproCell, Takara Bio Inc., and Fujifilm Holdings Corp.) fulfil the demand for HLCs in Asia, USA, and Europe. In general, bringing a new drug to market costs approximately \$800 million with approximately 10% market growth each year [50]. Pharmaceutical companies invest approximately \$1.5 billion to develop a new drug, and it usually takes 10-15 years before their drug is brought to market; nine out of ten drugs at clinical phase I will not pass marketing approval [51]. Approximately 20% of drugs demonstrate efficacy without any liver or cardiac toxicity during preclinical trials [52]. Finally, approximately 5% of candidate drugs in development can become licensed agents [53]. High research and development costs are leading to high drug prices, so it is important to develop methods for optimizing functional maturation of HLCs. At the same time, we should expand our knowledge of fundamental

differences between the latest HLCs and human primary hepatocytes used for *in vitro* and *in vivo* as well as clinical application.

FUTURE CHALLENGES AND SUGGESTIONS

Many researchers are interested in improving hepatic maturation of HLCs because they may open the door to a new cell source for drug screening and toxicity tests as well as for an alternative *in vitro* tool for animal studies. Additionally, many studies reported on a cell-cell interaction model that may mimic liver development with molecular markers to assess timing and intensity of *in vivo* transcriptional events. In our most recent study, we developed a novel strategy for enhancing hepatic maturation by applying a 3D culture system with repeated exposures of HLCs to xenobiotics

(Fig. 1)[8]. It was the first report to demonstrate that HLCs can be “educated,” suggesting that they can acquire a “learned” response to hepatotoxins.

Our strategy is based on the idea that hepatic metabolizing ability (activity of Phase I and II) has been primarily accomplished within the first three years of life. A neonate’s liver has only ~20% of the hepatocytes that will be present in the adult hepatocytes [54]. Therefore, the metabolizing rate and function of neonatal hepatocytes against to xenobiotics are low. Increased sensitivity of hepatocytes postnatally to xenobiotics may be due to repeated exposure to various xenobiotics, including those acquired through the diet early in life. This epigenetic modification method could induce expression and activities of hepatic metabolizing enzymes and thus produce highly functional HLCs for clinical application and *in vitro* toxicity screening.

According to our data, in addition to the ethnic variations between hESCs and hiPSCs, there are also biological variations regarding the efficiency of hepatic differentiation and gene expression profiling of hepatic metabolizing enzymes. Furthermore, the efficacy of one of the hiPSCs tested in our previous study was approximately 40%, indicating that potential tissue-specific genotypic variations of different hiPSC-derived HLCs exist. Therefore, when analyzing hepatotoxicity using HLCs, the ethnic and biological background of HLCs should be taken into account when making a rational and comprehensive decision.

Recently, in addition to HLCs derived from hESCs and hiPSCs, a population of liver stem cells has been identified by Nusse’s group [14]. Liver stem cells can proliferate and differentiate, giving rise to fully functional hepatocytes used to regenerate liver tissue. If we analyze and compare the similarities and differences among HLCs derived from hESCs and hiPSCs as well as newly identified liver stem cells, it may provide us with useful clues regarding maturing HLCs. In addition, it may provide information on how to delay or prevent degeneration of hepatic function and loss of hepatic characteristics in human primary hepatocytes.

CONCLUSION

The main concern in hepatic differentiation using human pluripotent stem cells is how to enhance the drug metabolizing ability of HLCs. Of the major drug metabolizing abilities of HLCs, phase I and II enzyme activity and MRPs are the focus of improvement efforts. Several previous studies have developed assays for these

hepatic enzymes and MRPs in human pluripotent stem cell-derived HLCs such as co-culture, 3D culture, and bioreactor. Mimicking *in vivo* liver development and functional maturation is the primary goal of these efforts. Unfortunately, many studies did not report promising outcomes, and their results indicate that there is still a long way to go towards enhancing drug metabolizing enzymes and MRPs in HLCs so that they are comparable to human primary hepatocytes. A key future task is developing a protocol to differentiate functionally mature hepatocytes derived from human pluripotent stem cells in sufficient numbers for clinical application. In order to accomplish this, a more solid understanding of cellular signal transduction, cell-cell interactions, cell-matrix interactions, and hepatic enzyme expression during liver development needs to be acquired, accompanied by stem cell research. In addition, functional comparisons between HLCs and human primary hepatocytes, liver stem cells, and *in vivo* liver are needed. Standardization of functional quality control of various phenotypes of HLCs for drug screening and testing (efficacy and toxicity) is needed for therapeutic application in the near future.

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